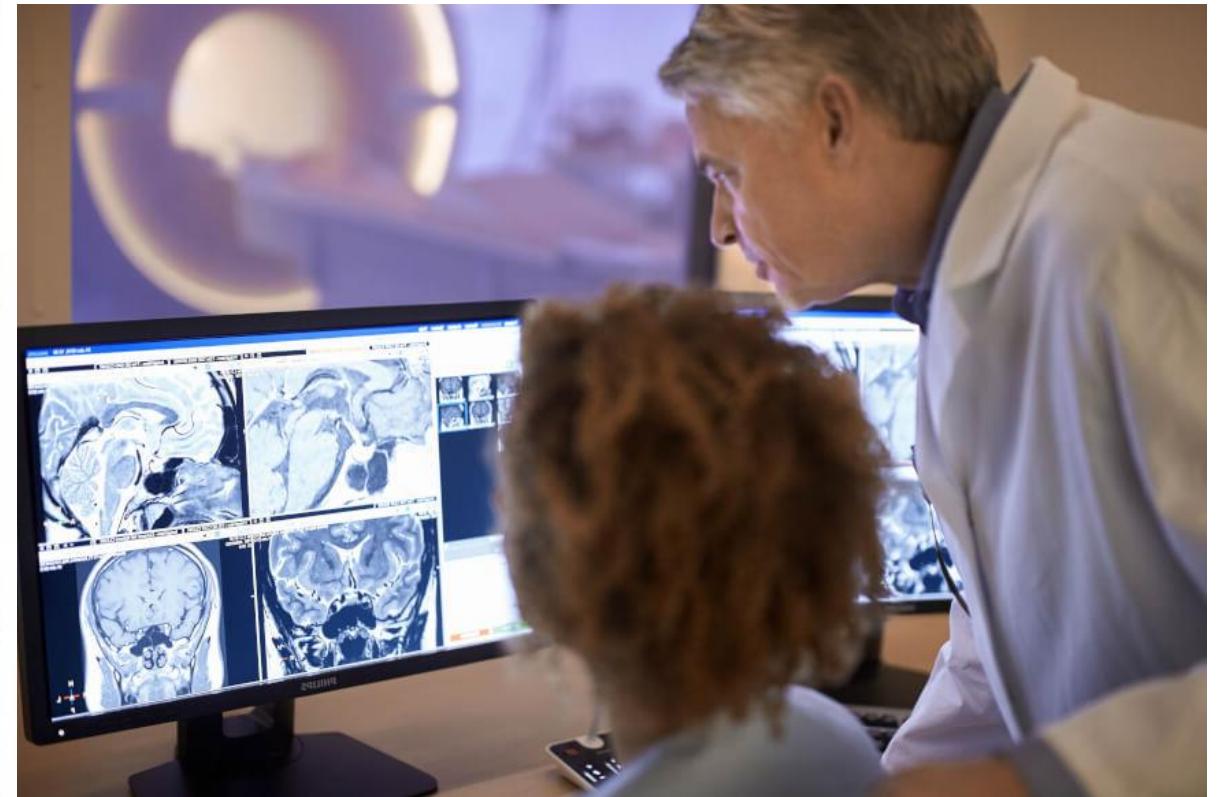


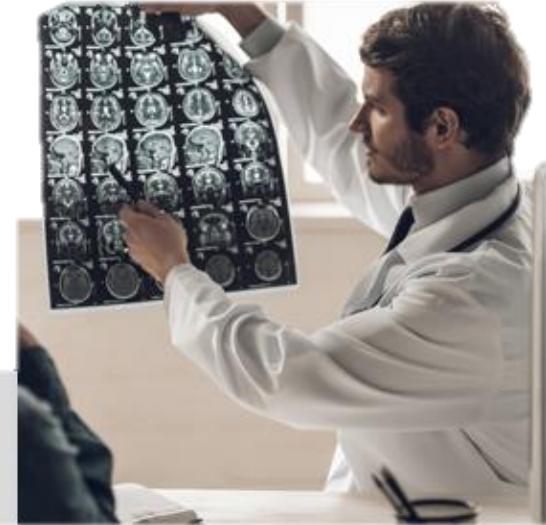


Laboratoire des sciences de l'ingénieur,
de l'informatique et de l'imagerie

Biomedical optical imaging : focus on clinical applications

Jean REHBINDER





MRI



Ultrasound



X-ray



CT-scanner

3D imaging of whole organs/ whole body
Mainly anatomical information,
sometimes functional (+ contrast agents)

Optics in medicine = low-tech?





Will light bring about the next
revolution in medical imaging?

- I. Some physics**
- II. Conventional optics and fluorescence**
- III. Optical Coherence Tomography (OCT)**
- IV. Non-Linear Microscopy (NLOM)**
- V. Polarimetry**
- VI. Summary**
- VII. Closing remarks**

Properties of light

Direction of propagation:

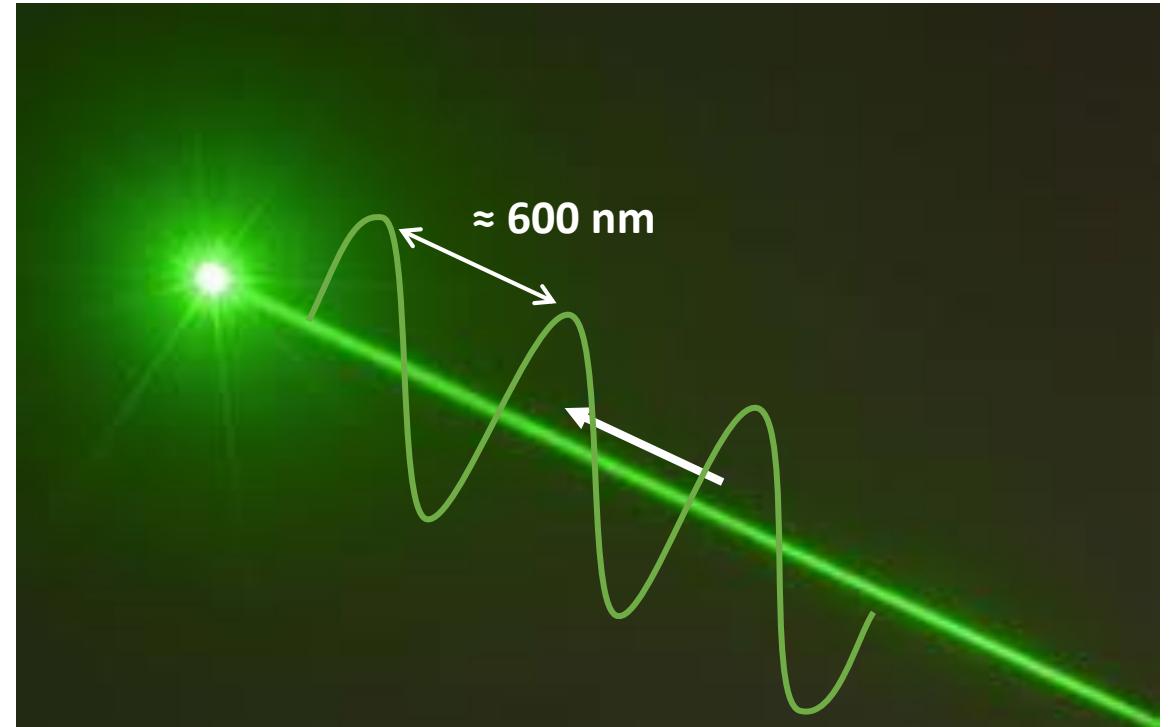
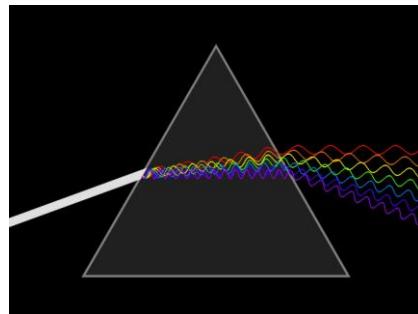
→ Geometrical optics
(lenses, microscope objectives,
endoscopes ...)

Wavelength (color):

→ Spectroscopy

Polarisation

→ Polarimetry



Properties of light

Direction of propagation:

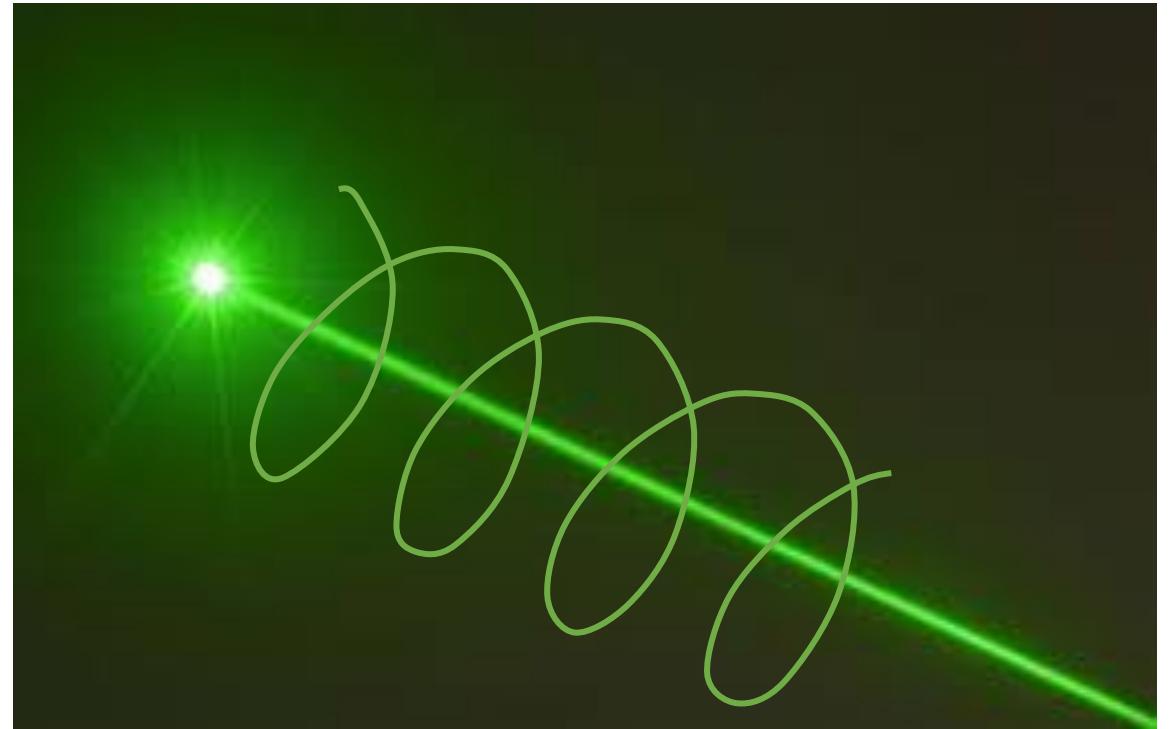
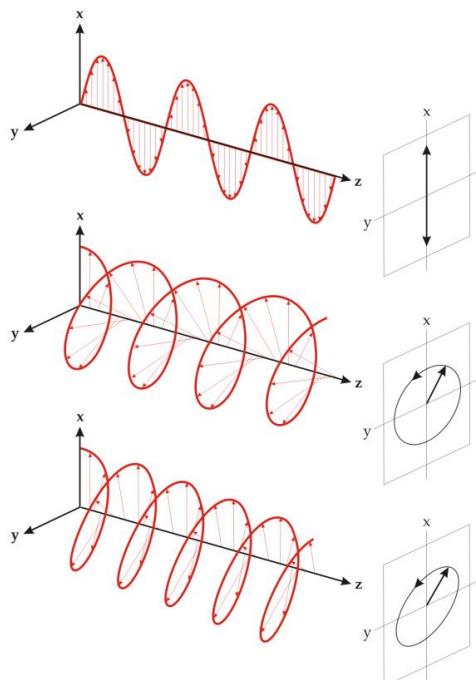
→ Geometrical optics
(lenses, microscope objectives,
endoscopes ...)

Wavelength (color):

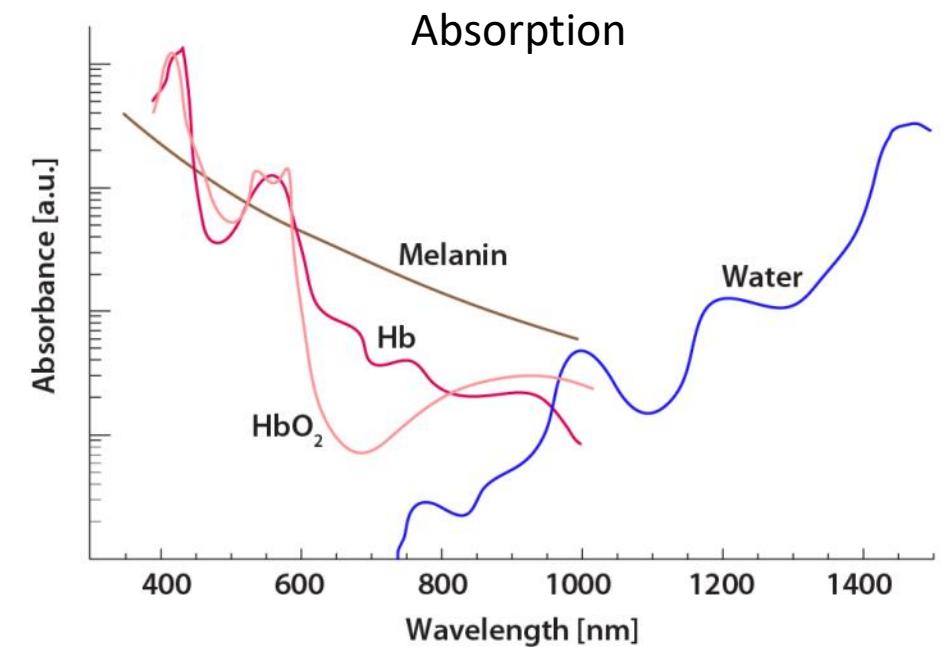
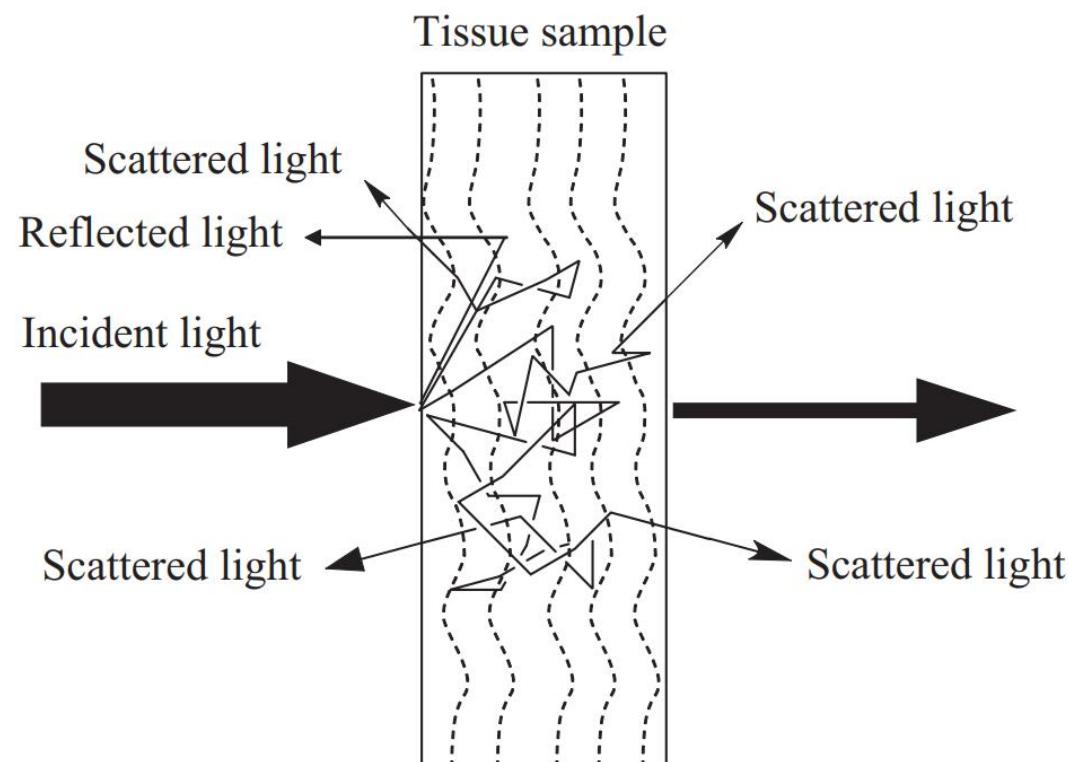
→ Spectroscopy

Polarisation

→ Polarimetry



Interaction of light with tissue



In biological tissues, scattering dominates over absorption

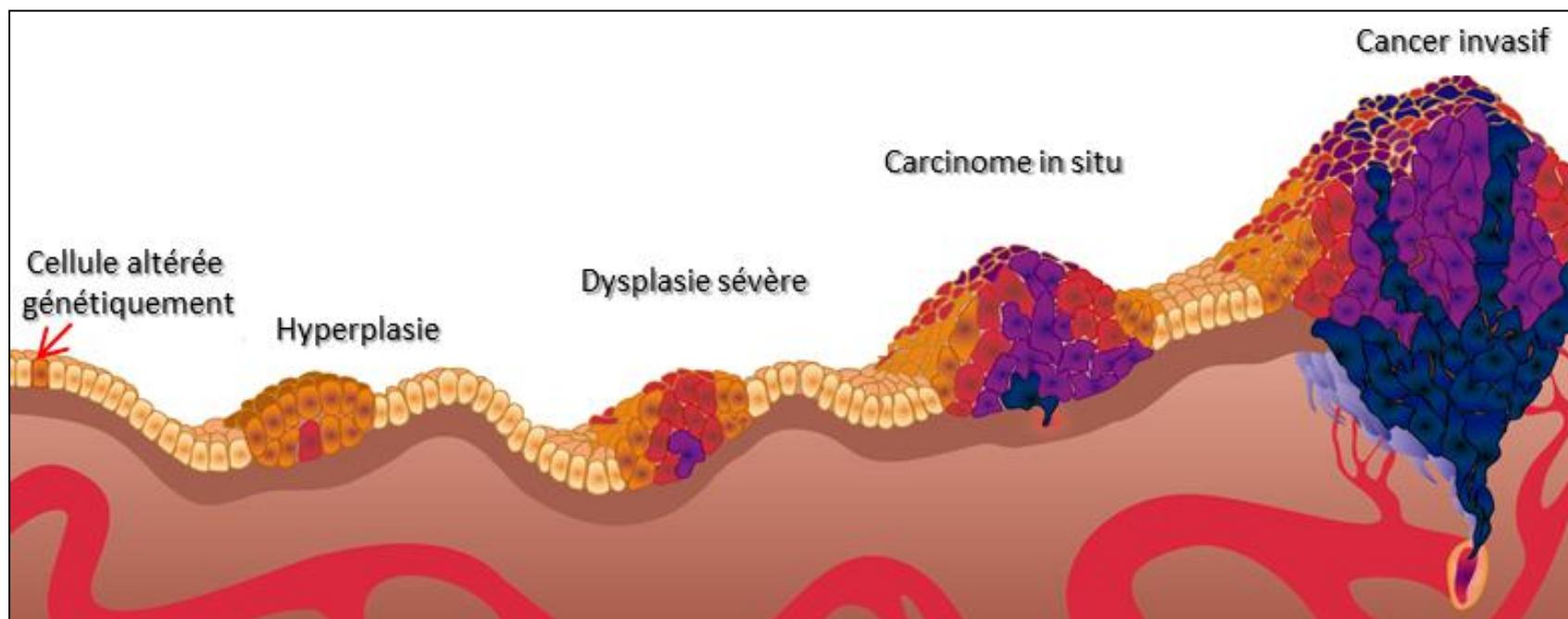
Penetration depth



Imaging typically limited to ≈ 1 mm depth
Scattering rapidly “blurs” the contrasts

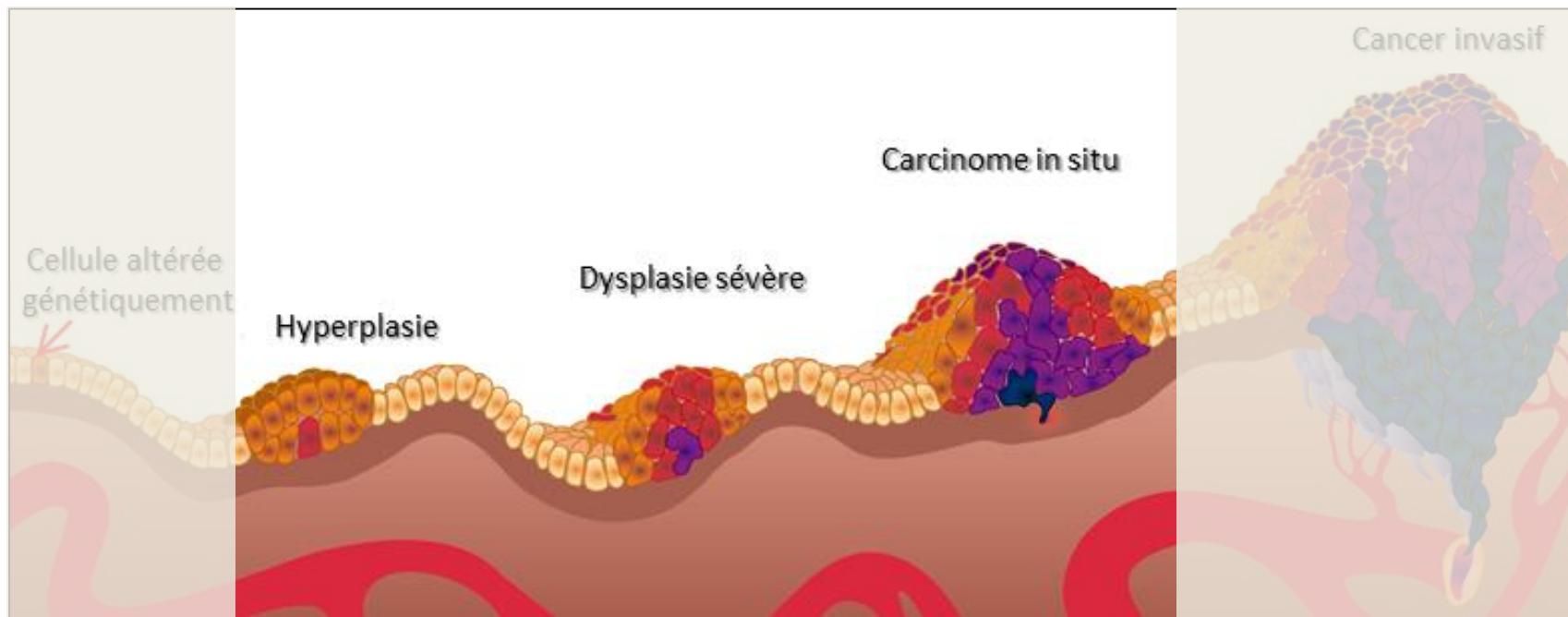
« Optical biopsy »

90% of cancers start from epithelia



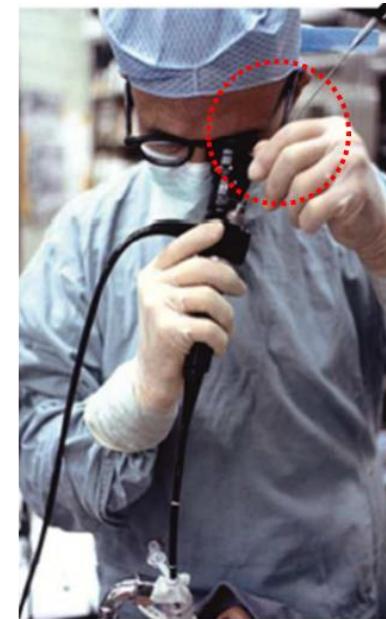
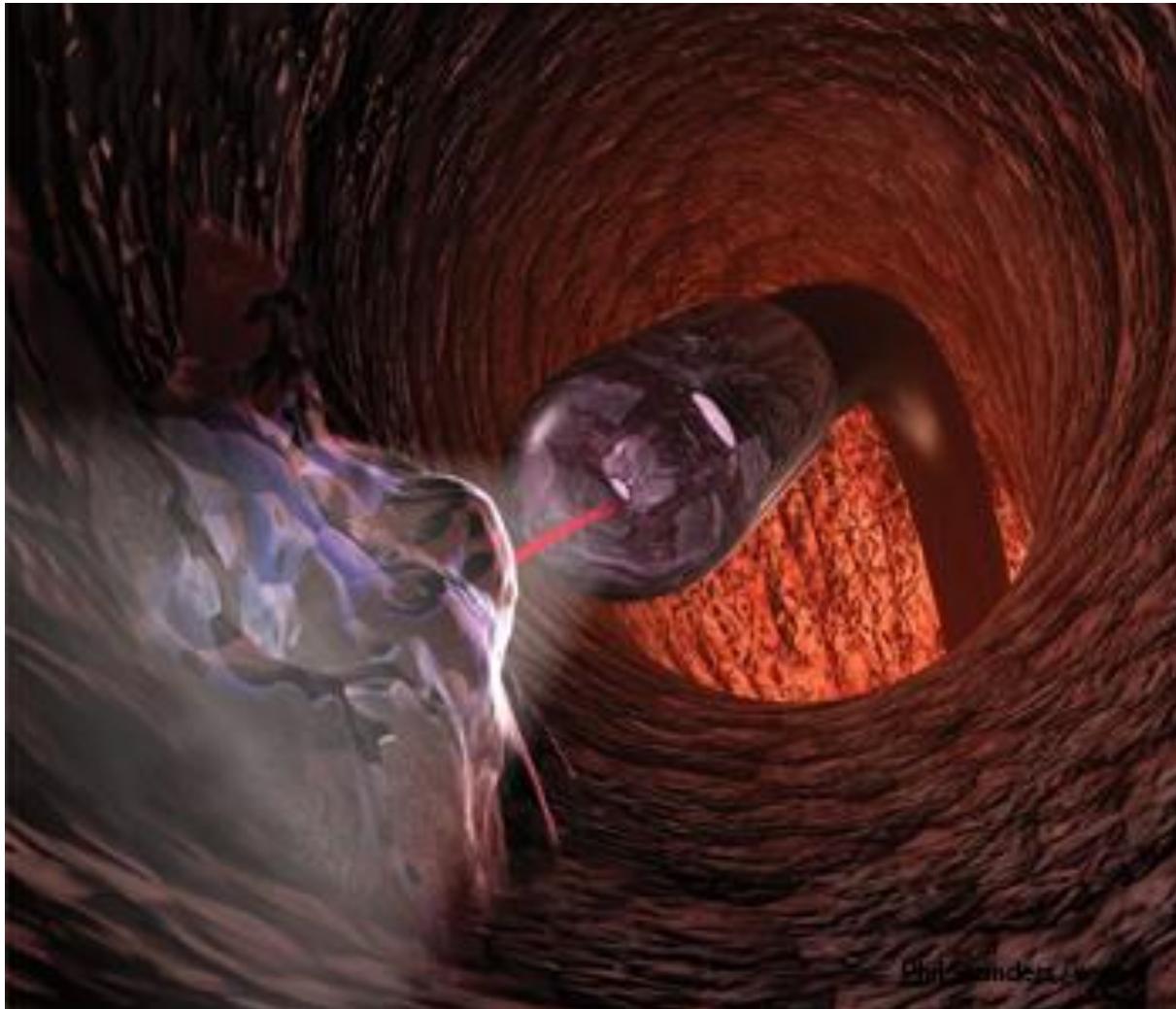
« Optical biopsy »

90% of cancers start from epithelia

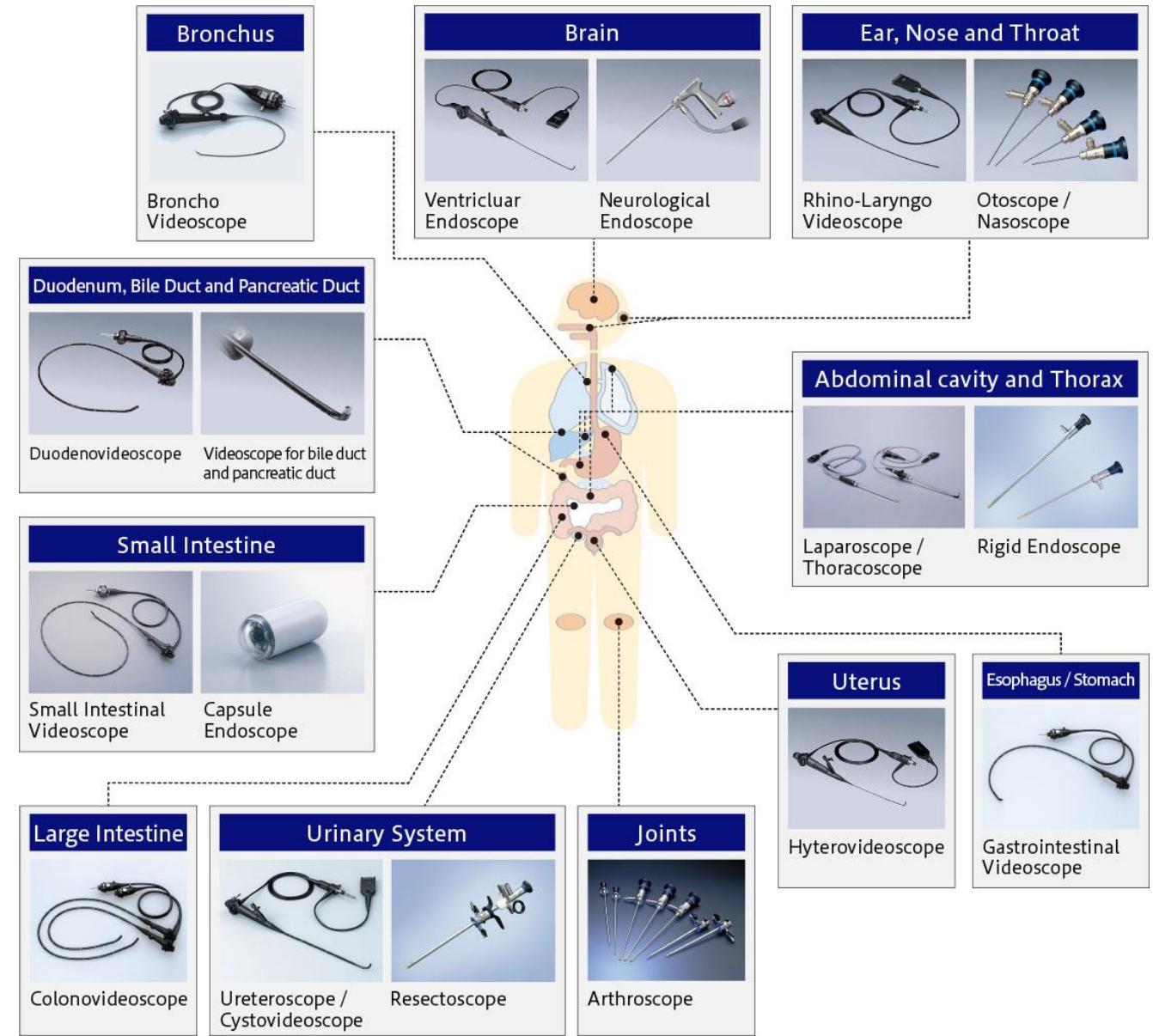
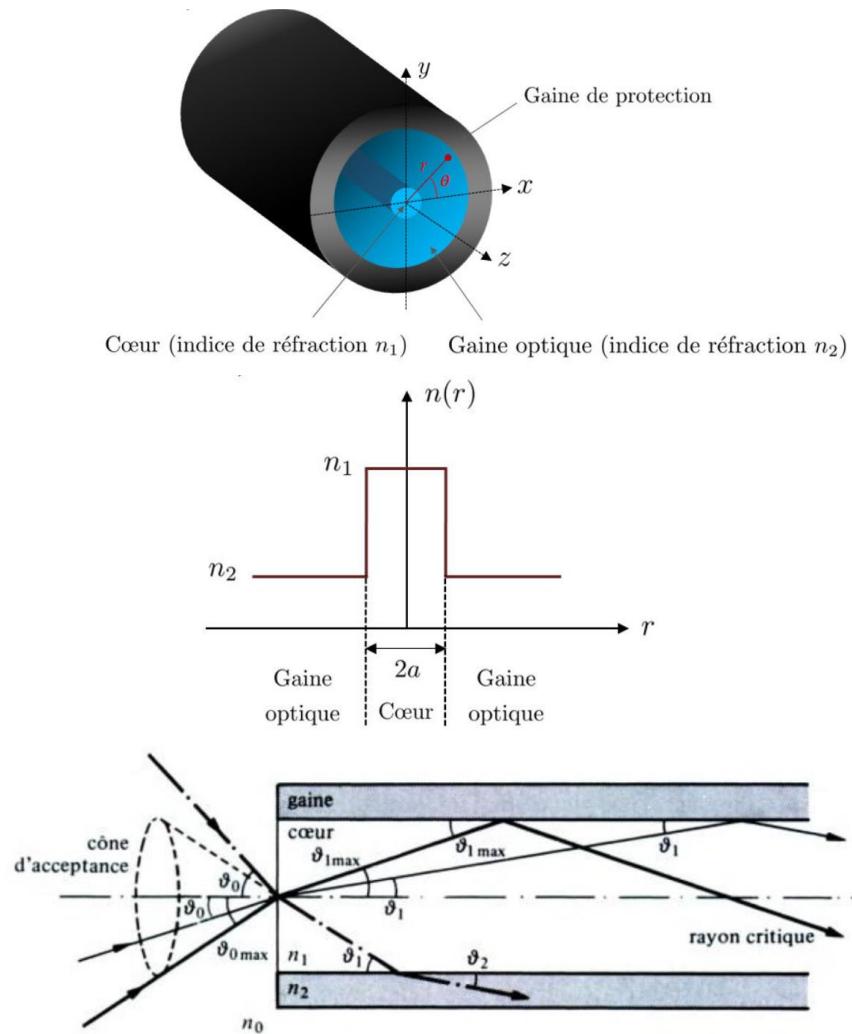


- I. Some physics
- II. Conventional optics and fluorescence
 - I. Principle
 - II. Instruments
 - III. Clinical applications
- IV. Example : a (French) research group or start-up
- III. Optical Coherence Tomography (OCT)
- IV. Non-Linear Microscopy (NLOM)
- V. Polarimetry
- VI. Summary
- VII. Closing remarks

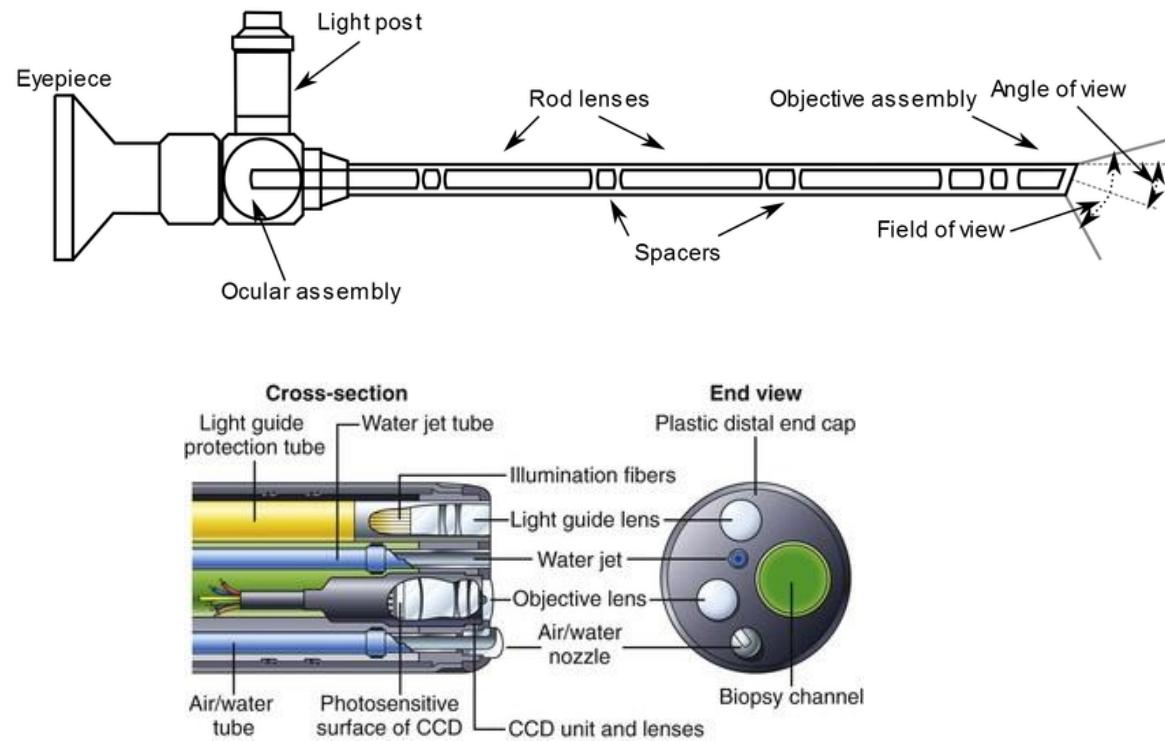
Endoscopy : bring light to the tissue



Endoscopes



Rigid endoscopes : minimally invasive surgery

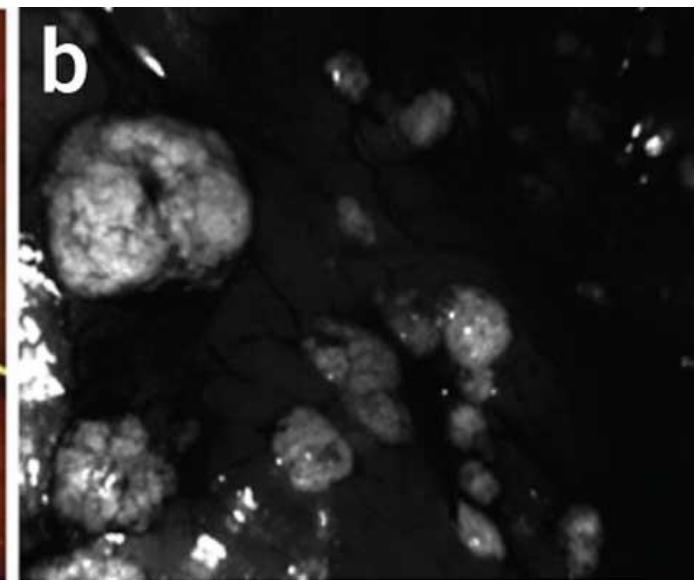
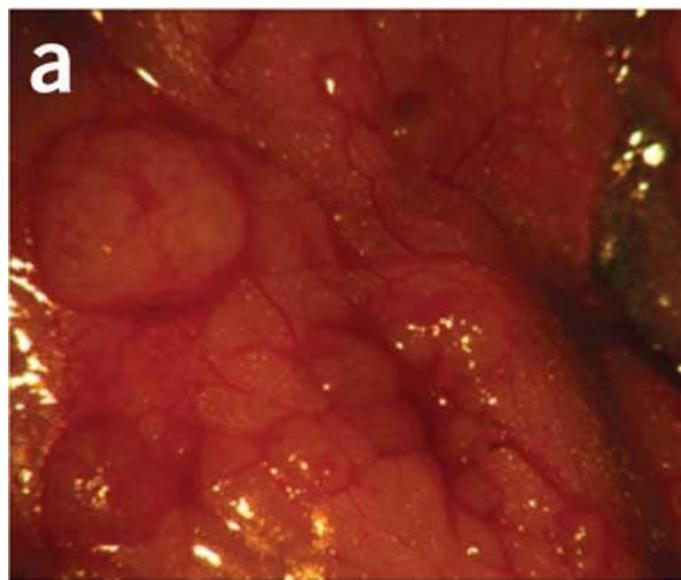
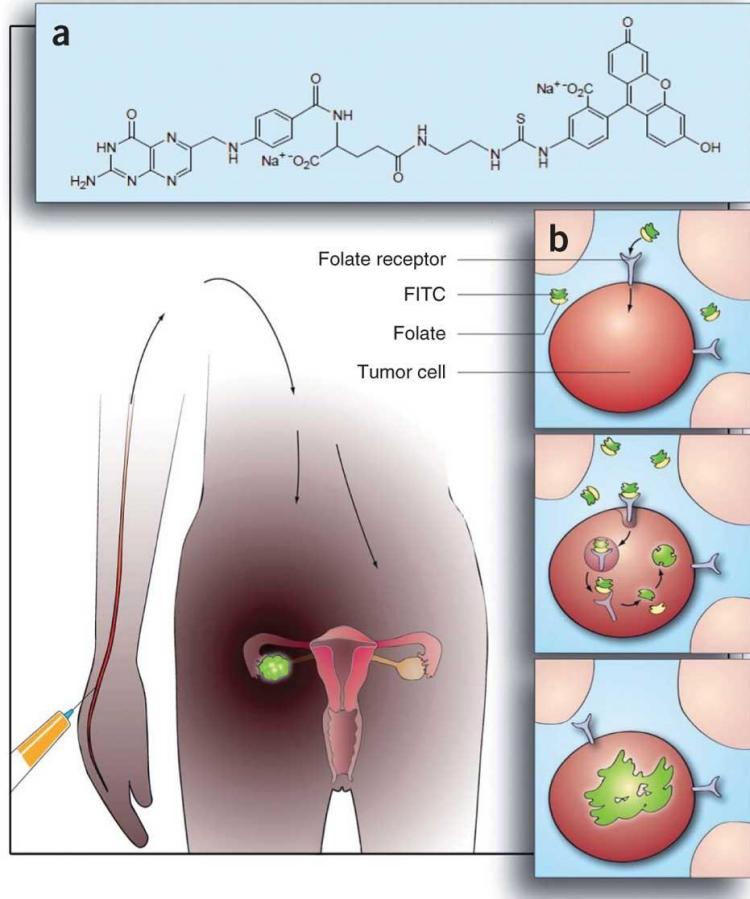


Wientjes, Rens, et al. "Automated objective routine examination of optical quality of rigid endoscopes in a clinical setting." *Plos one* 8.3 (2013): e59579.

<https://clinicalgate.com/how-endoscopes-work/>

Ponsky, T. A., & Ponsky, J. L. (2009). Advances in minimally invasive surgery. *Gastroenterology*, 136(4), 1171-1173.

Fluorescence



Mauna Kea Technologies



pCLE (probe / catheter)



nCLE (needle)

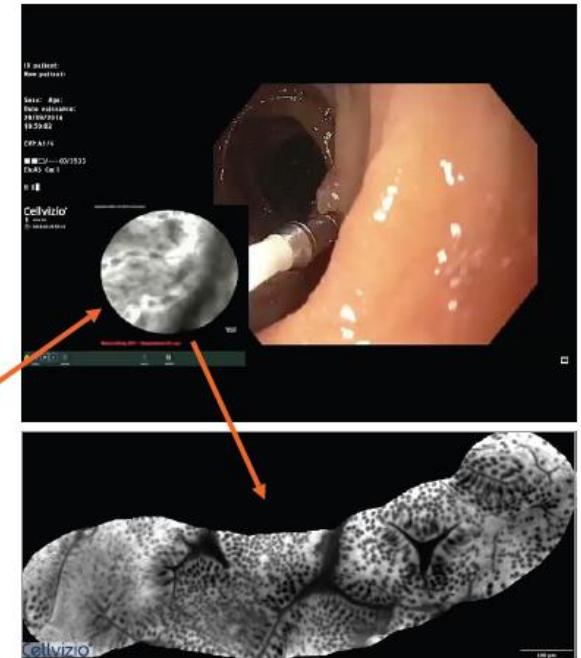
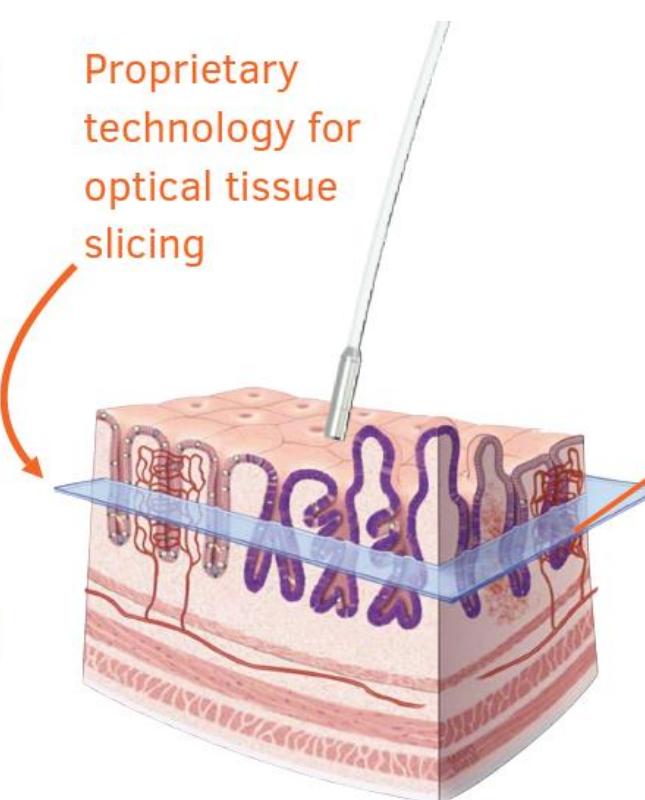


pCLE (lap / robotics)



Clinical
Cellvizio®
Platform

Miniprobes
for various access
methods (0.8 to 2.5 mm)



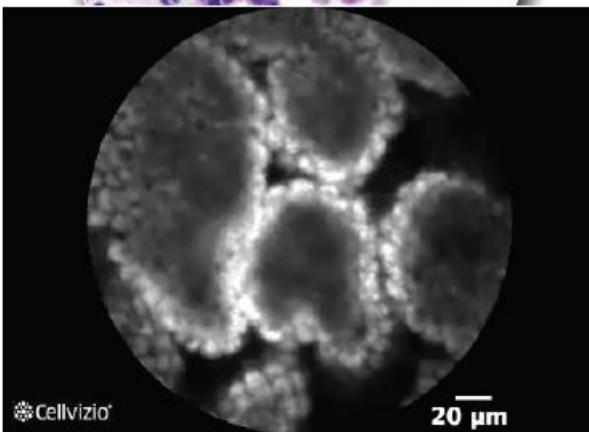
Breakthrough Confocal Laser Endomicroscopic scanning through 30,000 custom optical fibers produces 12 microscopic optical sections per second during standard endoscopy procedures

Real-time *in-vivo* microscopy

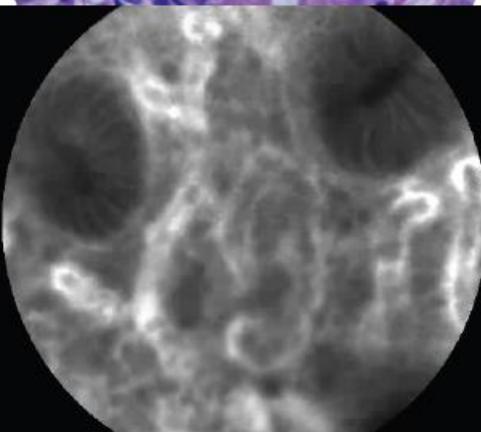
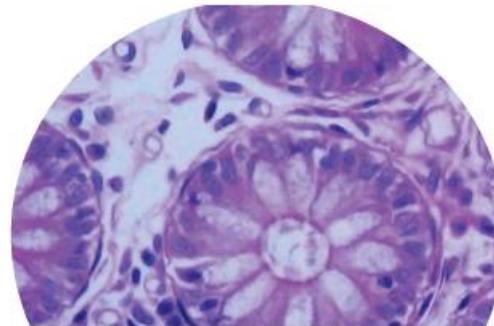
From H&E histology...
one image - static view



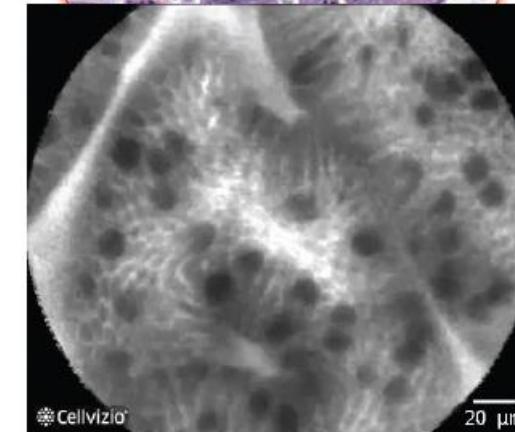
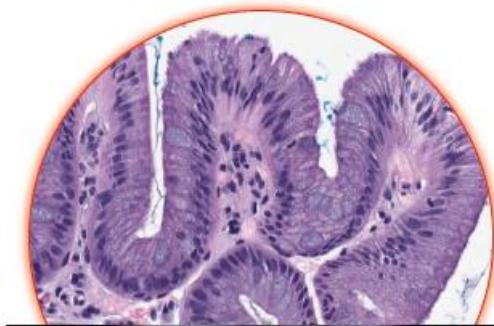
...to Cellvizio®
720 live
microscopic
images per
minute -
functional view



Brain



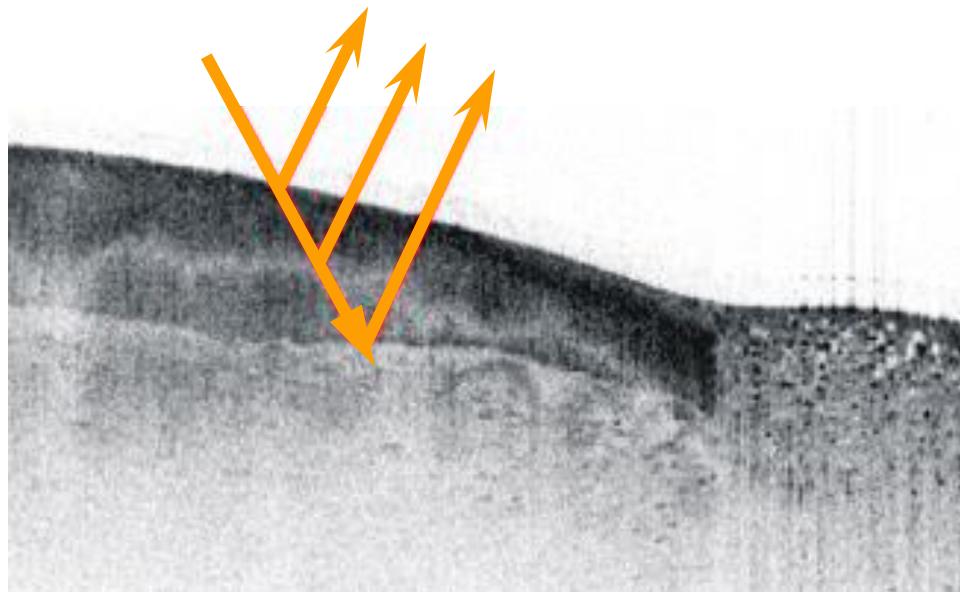
Colon



Esophagus

Optical Coherence Tomography (OCT)

Similar principle to ultrasonography ... but with light!

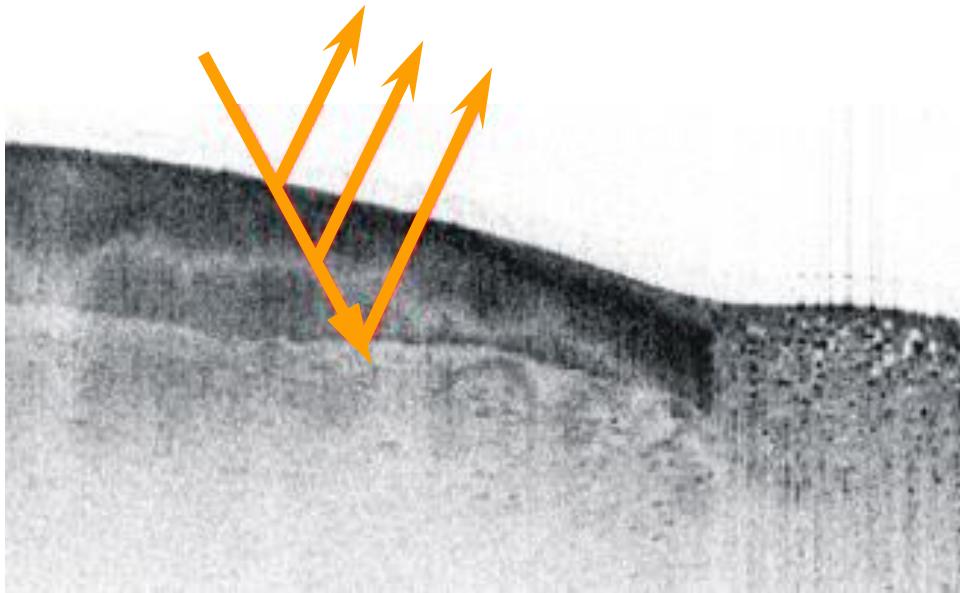


Ultrasound: 1-20 MHz – 1540 m/s
→echo detected with electronic transducers

Visible light: 375-750 THz – $3 \cdot 10^8$ m/s !

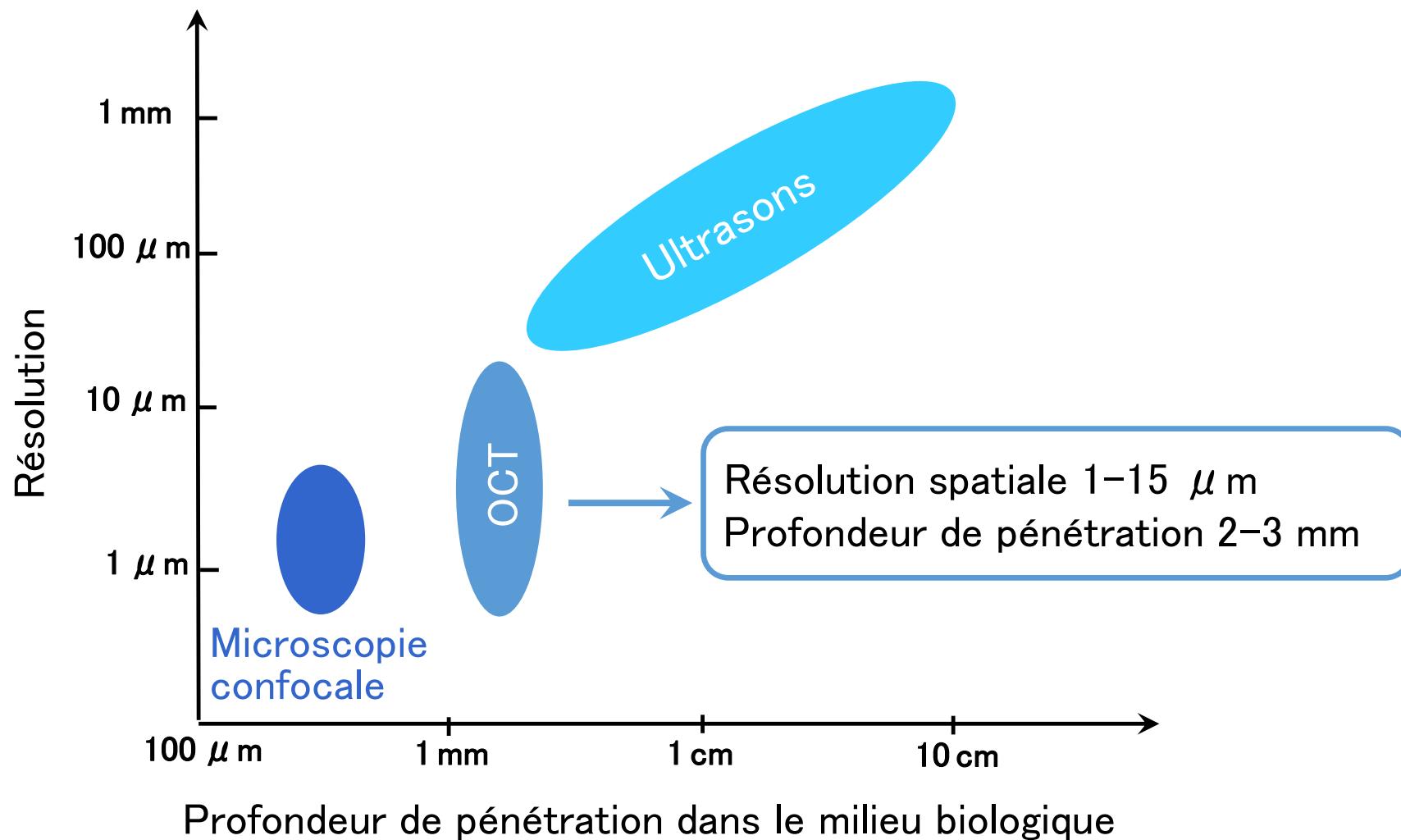
Optical Coherence Tomography (OCT)

Similar principle to ultrasonography ... but with light!

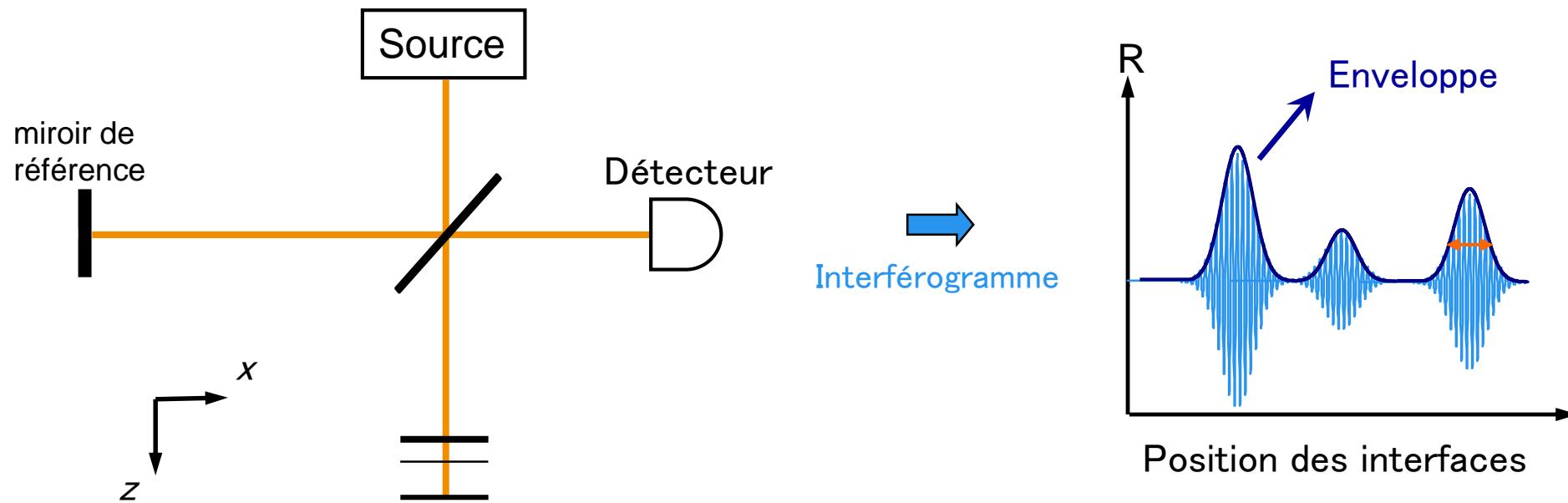


Principle: interferometric measurement of the amplitude and travel time of light backscattered by the biological medium

OCT : unique properties

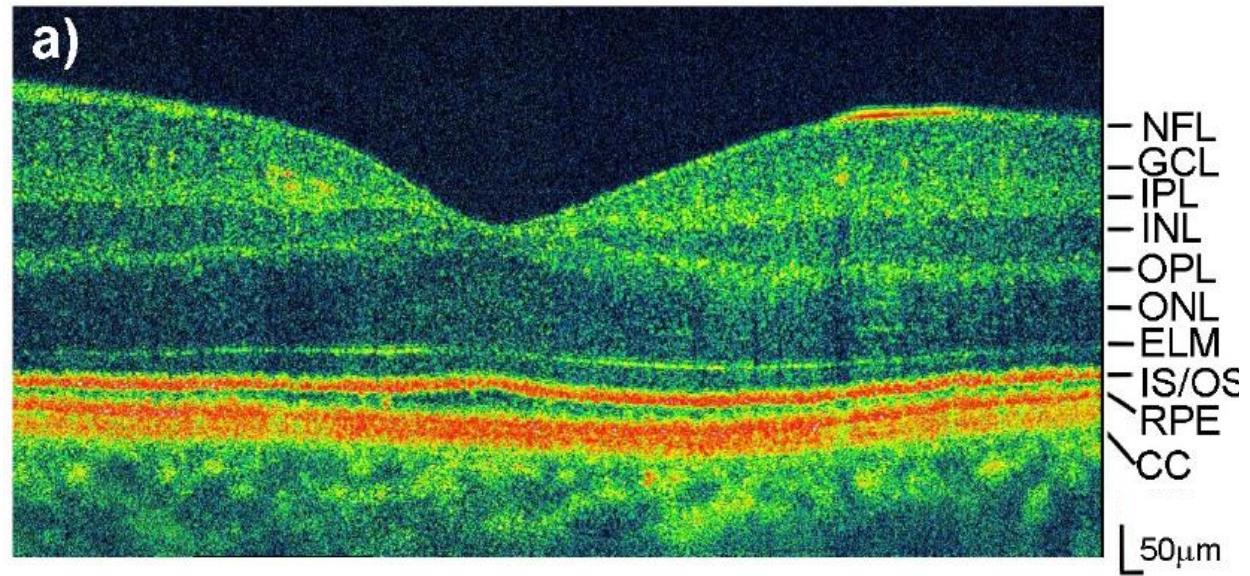


OCT : working principle



- distribution des structures selon z obtenue par balayage de la différence de marche
- distribution des structures selon x et y obtenue par balayage 2D du faisceau

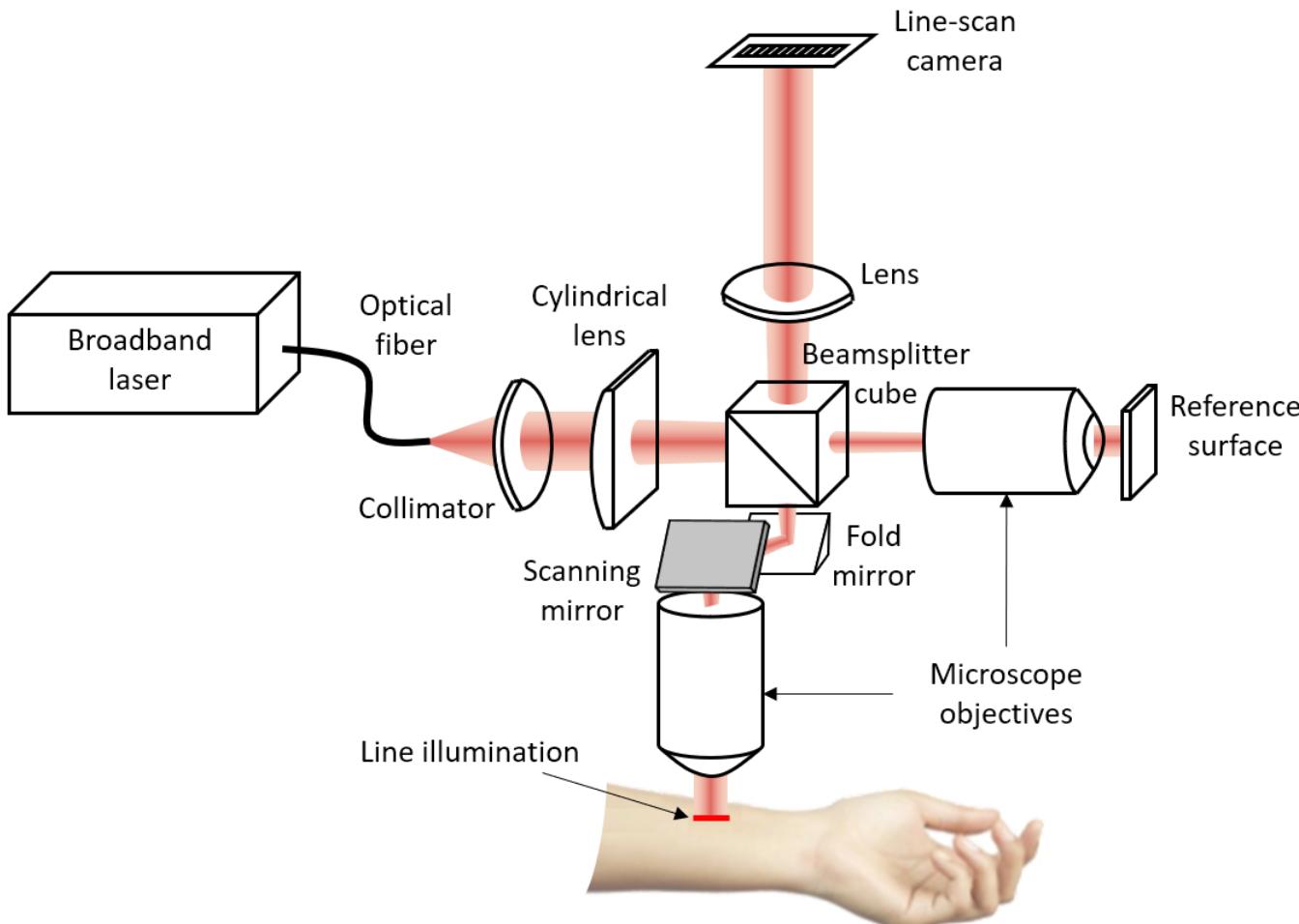
Success story : OCT for ophthalmology



Wojtkowski, M., Srinivasan, V. J., Ko, T. H., Fujimoto, J. G., Kowalczyk, A., & Duker, J. S. (2004). Ultrahigh-resolution, high-speed, Fourier domain optical coherence tomography and methods for dispersion compensation. *Optics express*, 12(11), 2404-2422.

Damae Medical

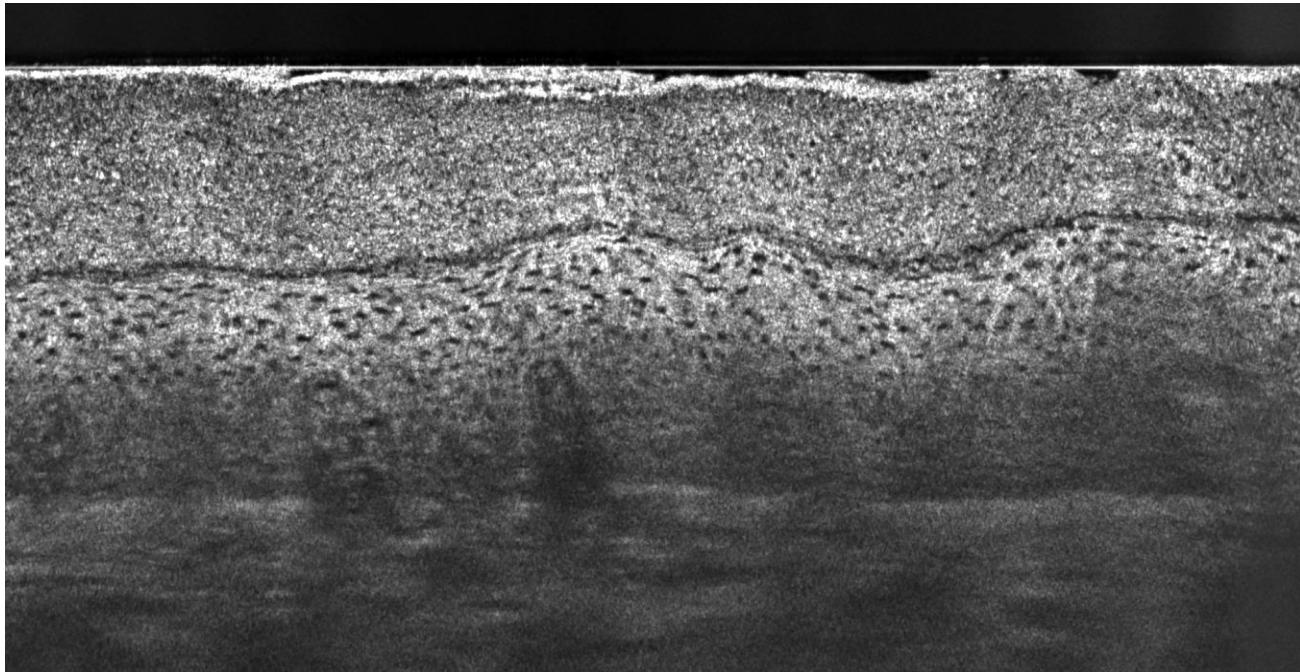
Line-Field Confocal Optical Coherence Tomography



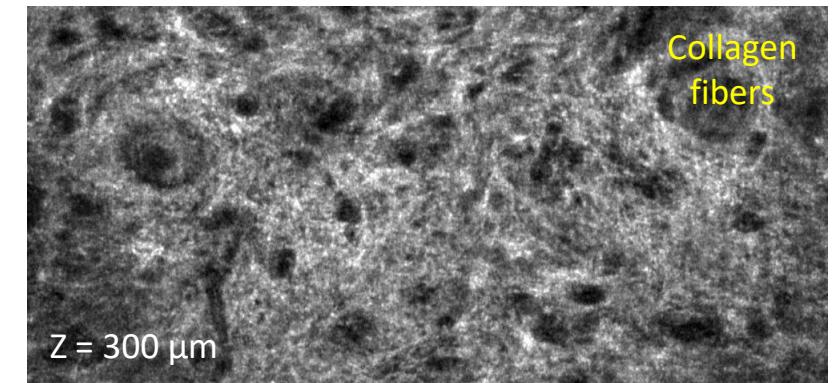
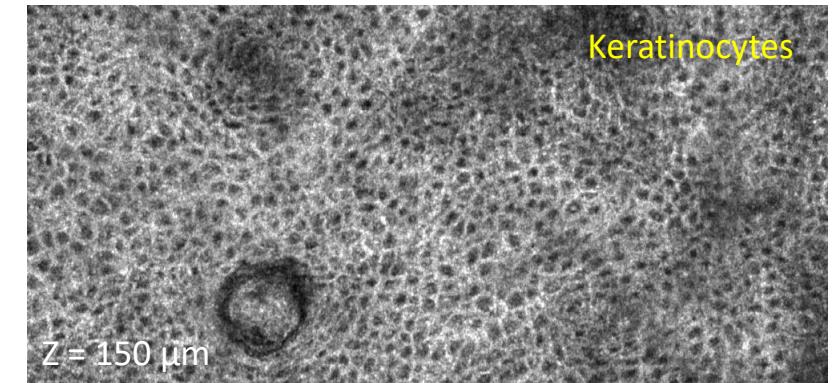
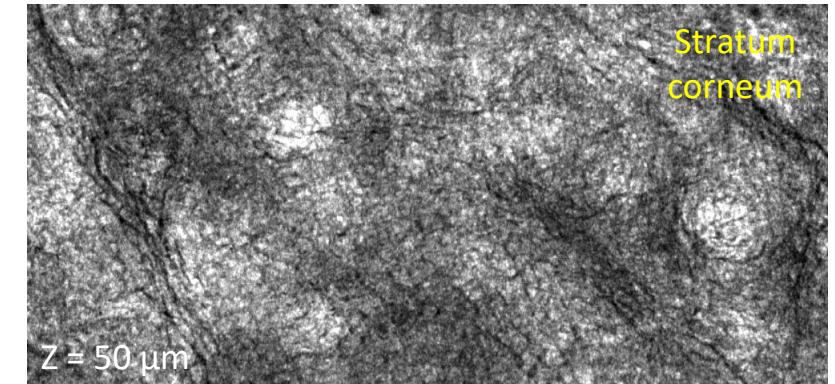
Technology invented by Pr. Arnaud Dubois
(CNRS, IOGS, UPSaclay)
Fully transferred to DAMEE Medical



Healthy skin

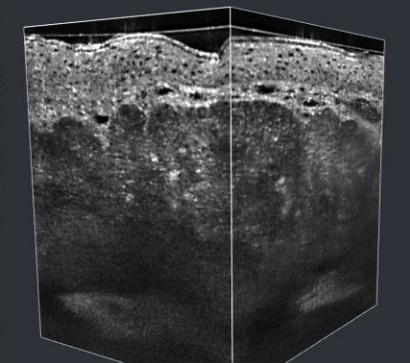
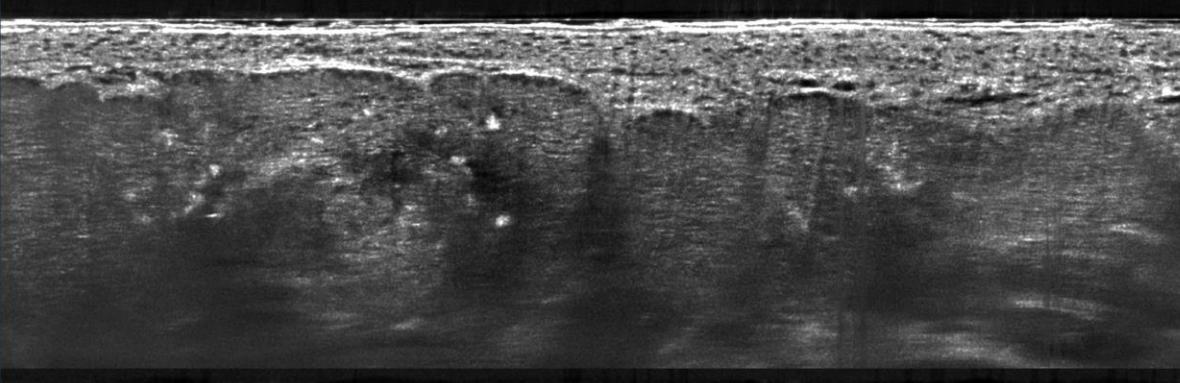
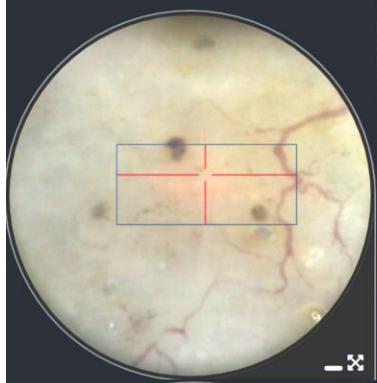


Horizontal sections

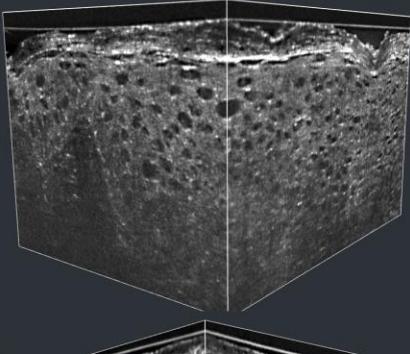
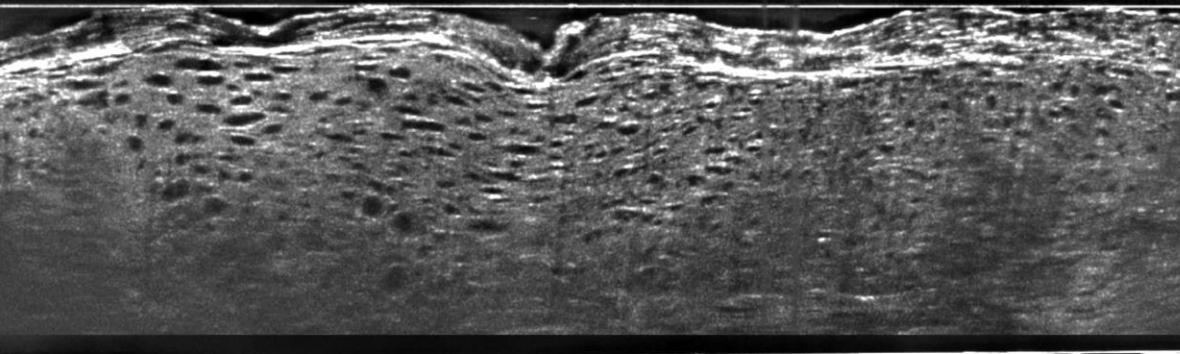
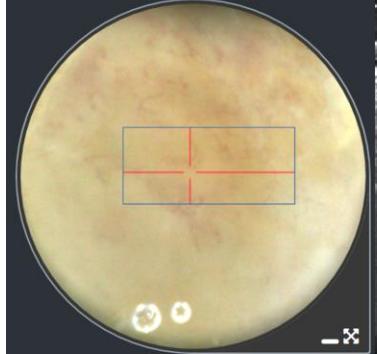




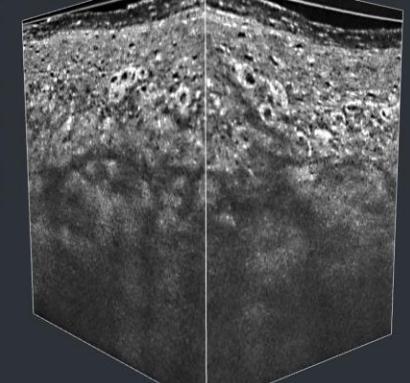
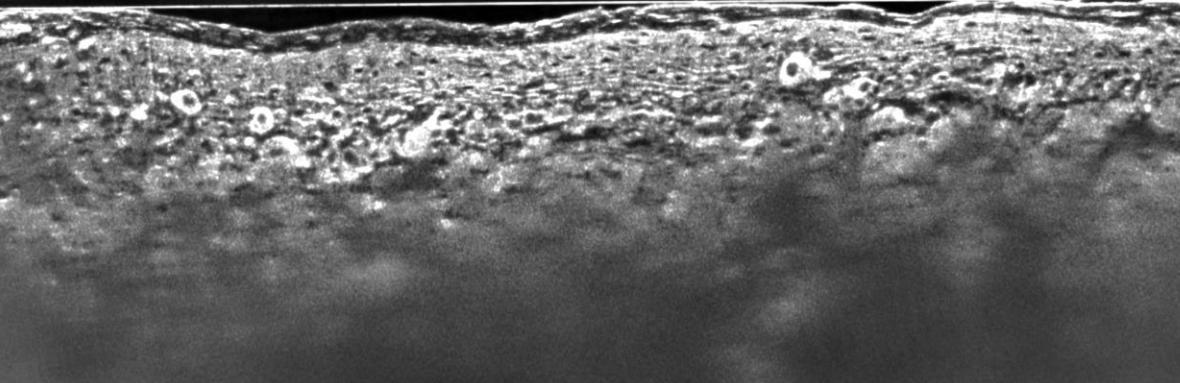
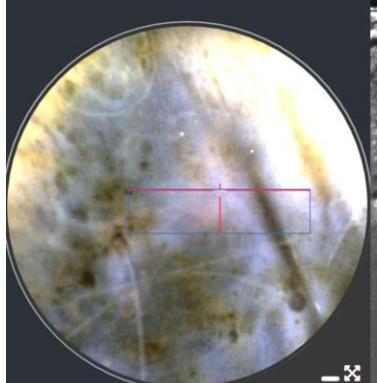
- **Cellular resolution** (~ 1 μm , isotropic)
 - **Live vertical imaging mode** (1.2 mm x 0.4 mm, 8 fps)
 - **Live horizontal imaging mode** (1.2 mm x 0.5 mm, 8 fps)
 - **3D imaging mode** (1.2 mm x 0.5 mm x 0.5 mm, 30 s)
- + video-dermoscopy (resolution: 5 μm ; field of view: 2.5 mm)**



**Basal Cell
Carcinoma**



**Squamous cell
carcinoma**



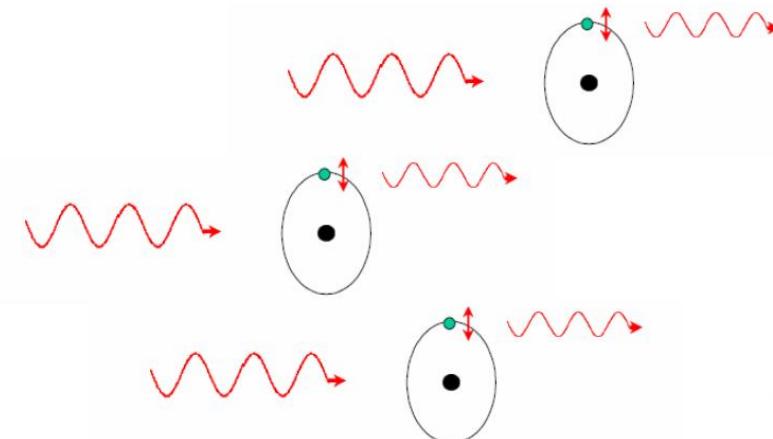
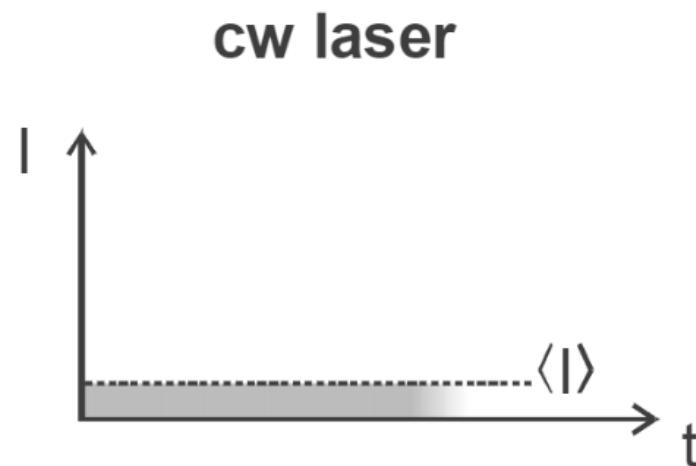
Melanoma

Video-dermoscopy

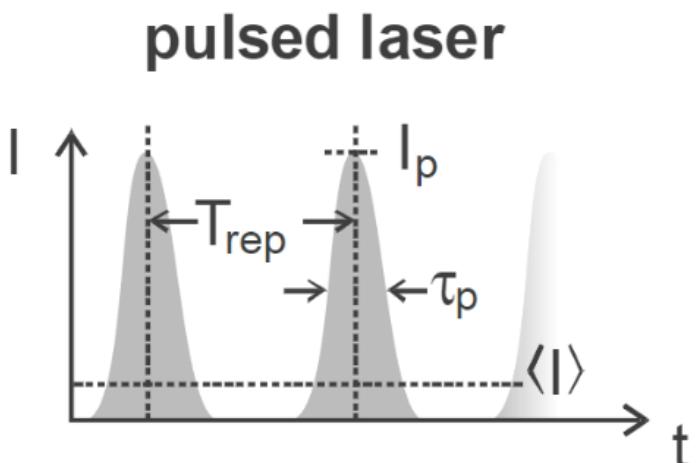
Vertical section

3D

Non-Linear Optical Microscopy



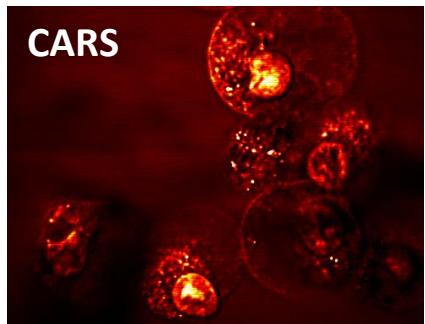
Linear Effects :
- Absorption
- Scattering
 $\text{Signal} \propto I$



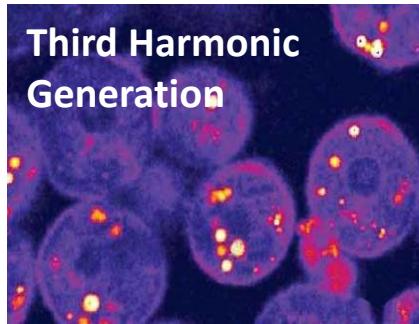
$$\vec{P}(t) = \varepsilon_0(\chi^{(1)}\vec{E} + \chi^{(2)}\vec{E}\vec{E} + \chi^{(3)}\vec{E}\vec{E}\vec{E} + \dots)$$

→ Non-Linear Effects :
 $\text{Signal} \propto I^{(n)}$

Non-linear optical effects



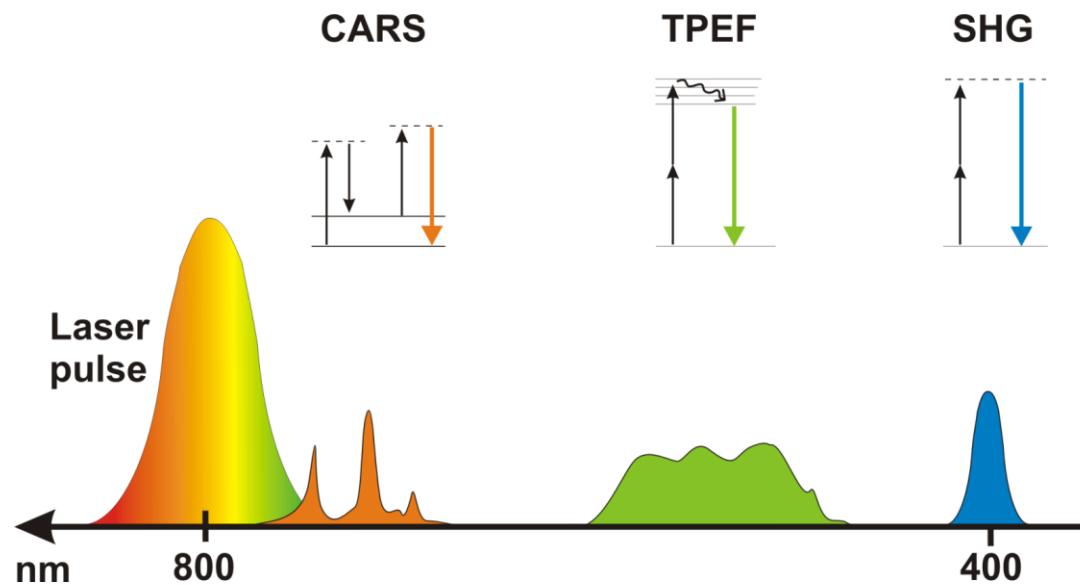
Cheng et al., *Biophys. J.*
83, 502 (2002).



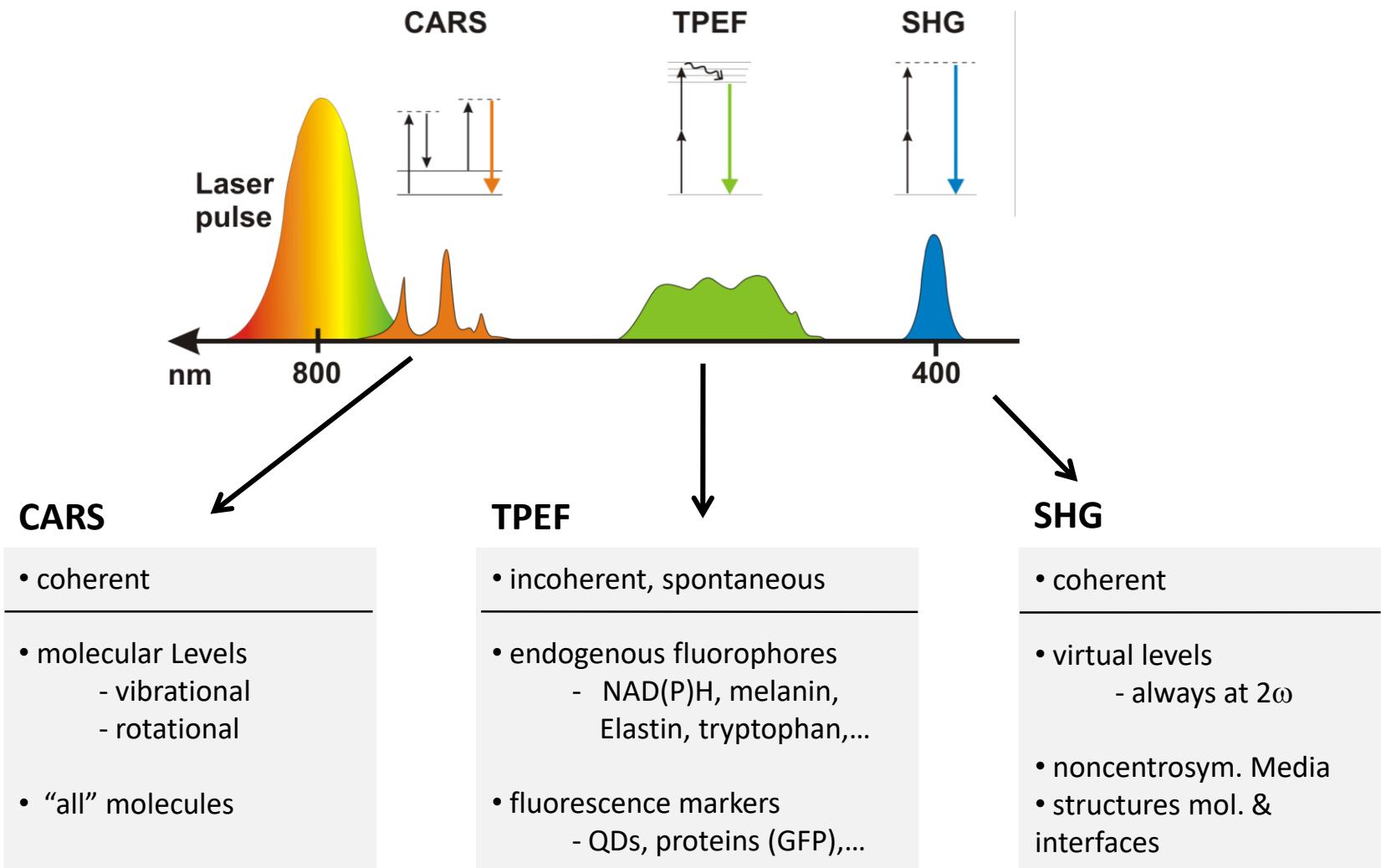
Débarre et al., *Nature Methods* **3**, 47 (2006).



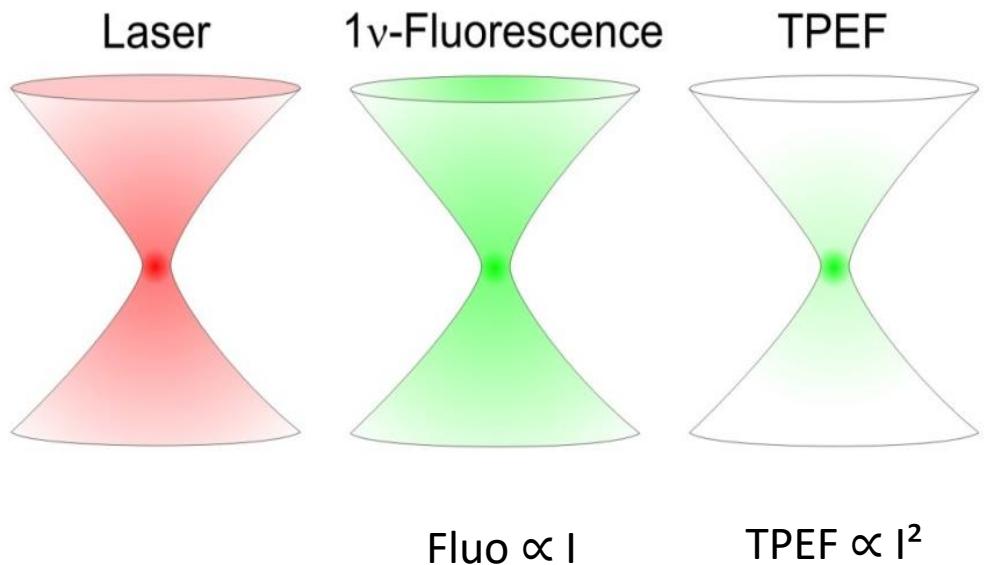
Zipfel et al., *Nature Biotech.*
21, 1369 (2003).



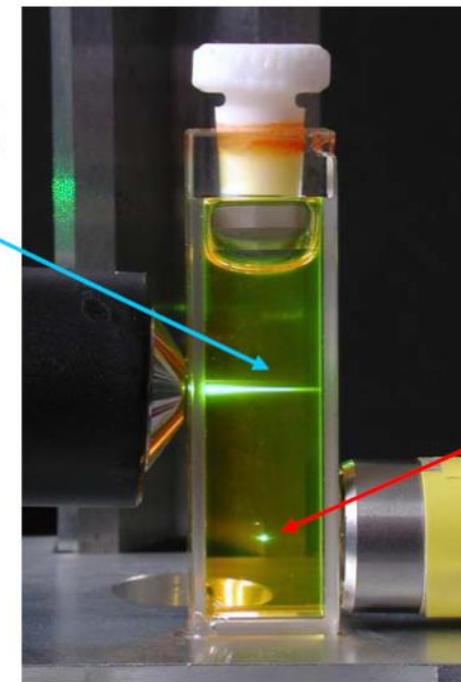
Chemical & microstructural sensitivity



Inherent 3D capability

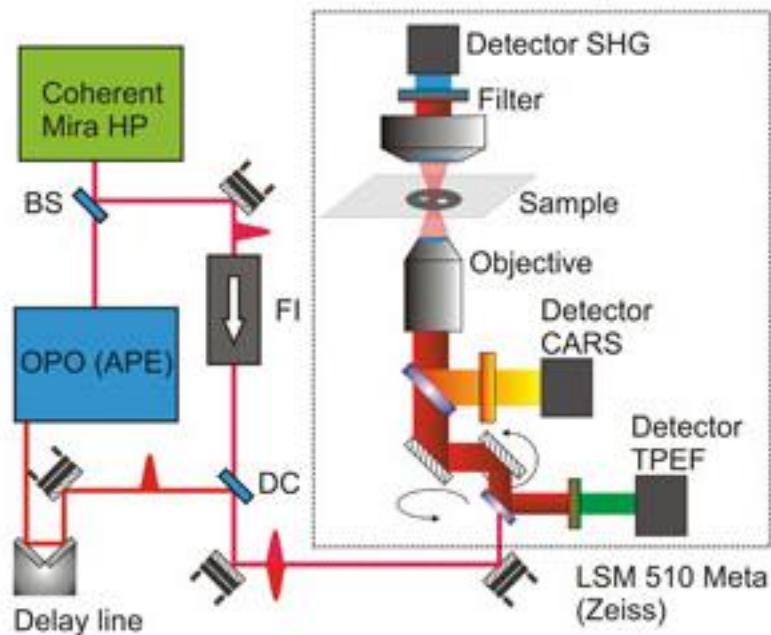


Fluorescence suite
à une absorption à
un photon



Fluorescence suite
à une absorption à
deux photons

NLOM setup



Challenging technique :

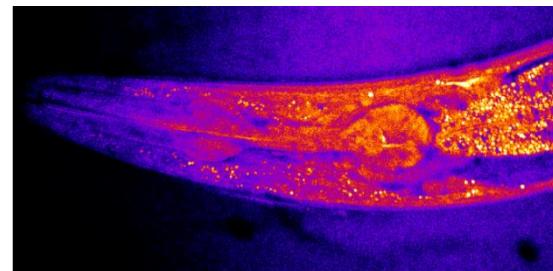
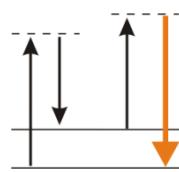
- ps- or fs-lasers
- precise optical alignment
- Rapid scanning
- Filters and detectors

LOB – Ecole polytechnique

Biological processes at the sub-cellular level revealed through non-linear microscopy

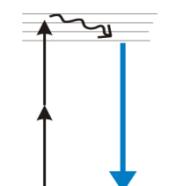
C. elegans worm

CARS



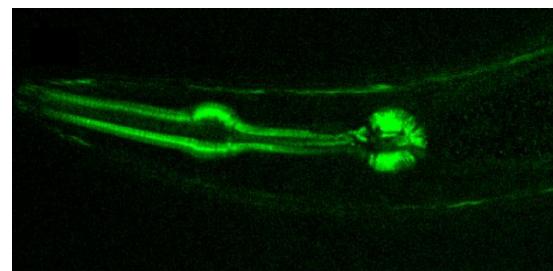
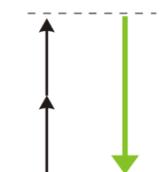
epithelial lipids

TPEF



fluorescent vesicles

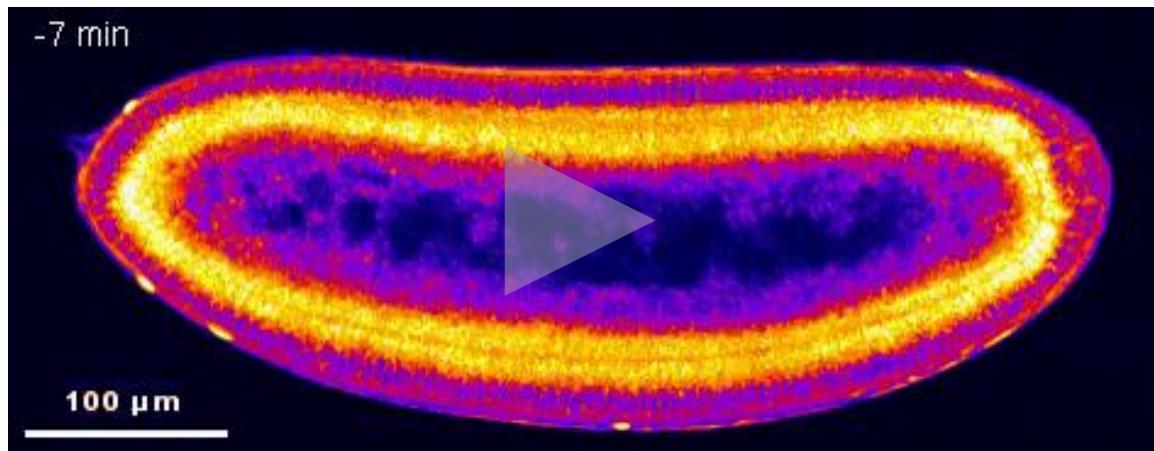
SHG



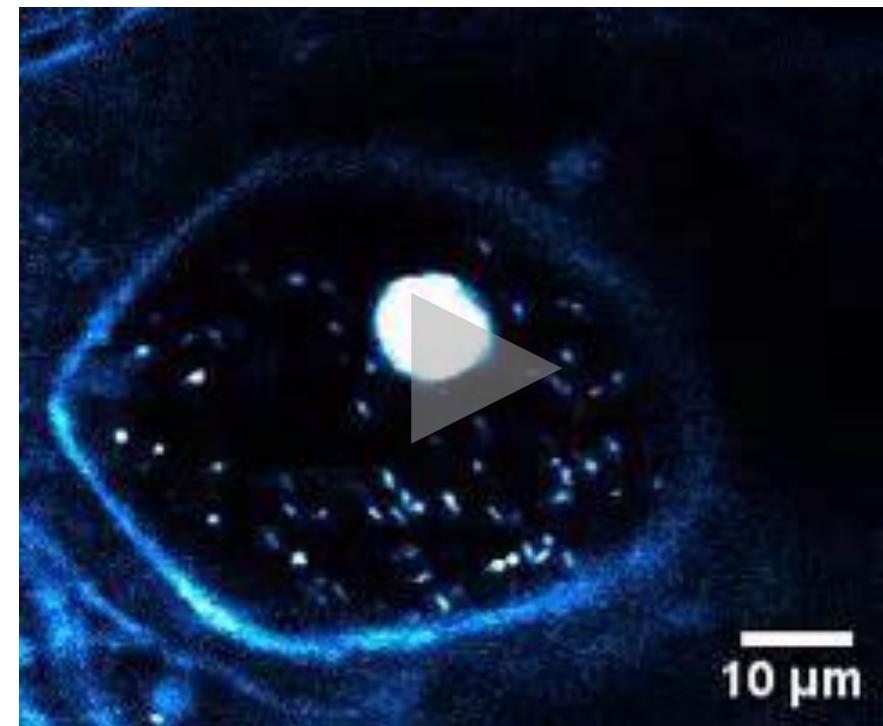
muscles

LOB – Ecole polytechnique

Biological processes at the sub-cellular level revealed through non-linear microscopy

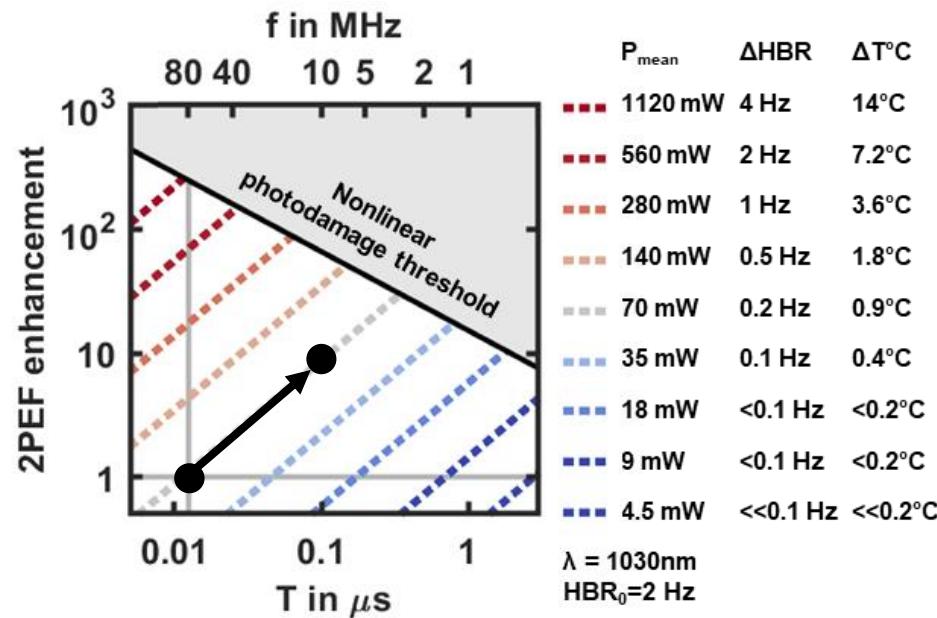


Supatto, Willy, et al. "In vivo modulation of morphogenetic movements in Drosophila embryos with femtosecond laser pulses." *Proceedings of the National Academy of Sciences* 102.4 (2005): 1047-1052.



THG imaging of flowing endogenous microparticles in the otolith cavity of a zebrafish.
Excitation power: 100-150 mW. Axial resolution: 2μm. Time per pixel: 10 μ s. Time between images: 620 ms. Typical signal level (particles): 30-80 photons

Photodamage mitigation



$$2\text{PEF signal enhancement} = T P_{mean}^2 / T_0 P_0^2$$

$$T_0 = 1/80\text{MHz}$$
 and $P_0 = 70\text{mW}$

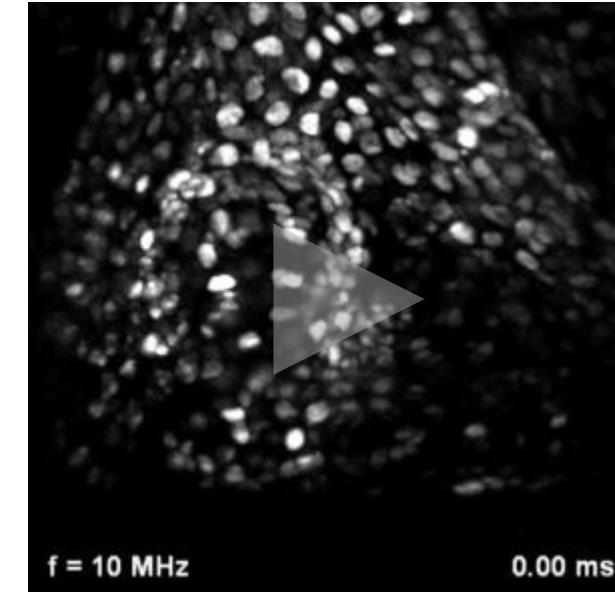
On this graph: n_D -order Damage threshold $\sim T^{2/n_D-1}$

Strategy

Decrease $f=1/T$ to $\sim 10\text{ MHz}$ at constant P_{mean}

- ▶ 8x 2PEF enhancement
- ▶ $\Delta T^\circ C < 1^\circ C$
- ▶ Still far from nonlinear photodamage

Best compromise!



Zebrafish beating heart | mCherry | $\lambda=1030\text{nm}$
@170 fps / 40MHz pixel rate

8x 2PEF signal enhancement

FOV 200 x 200 μm

My journey with polarimetry

1. PostDoc project 2013-2017

Team of Angelo Pierangelo

- Early detection of cervical cancer
- Diagnosis of risk of premature delivery



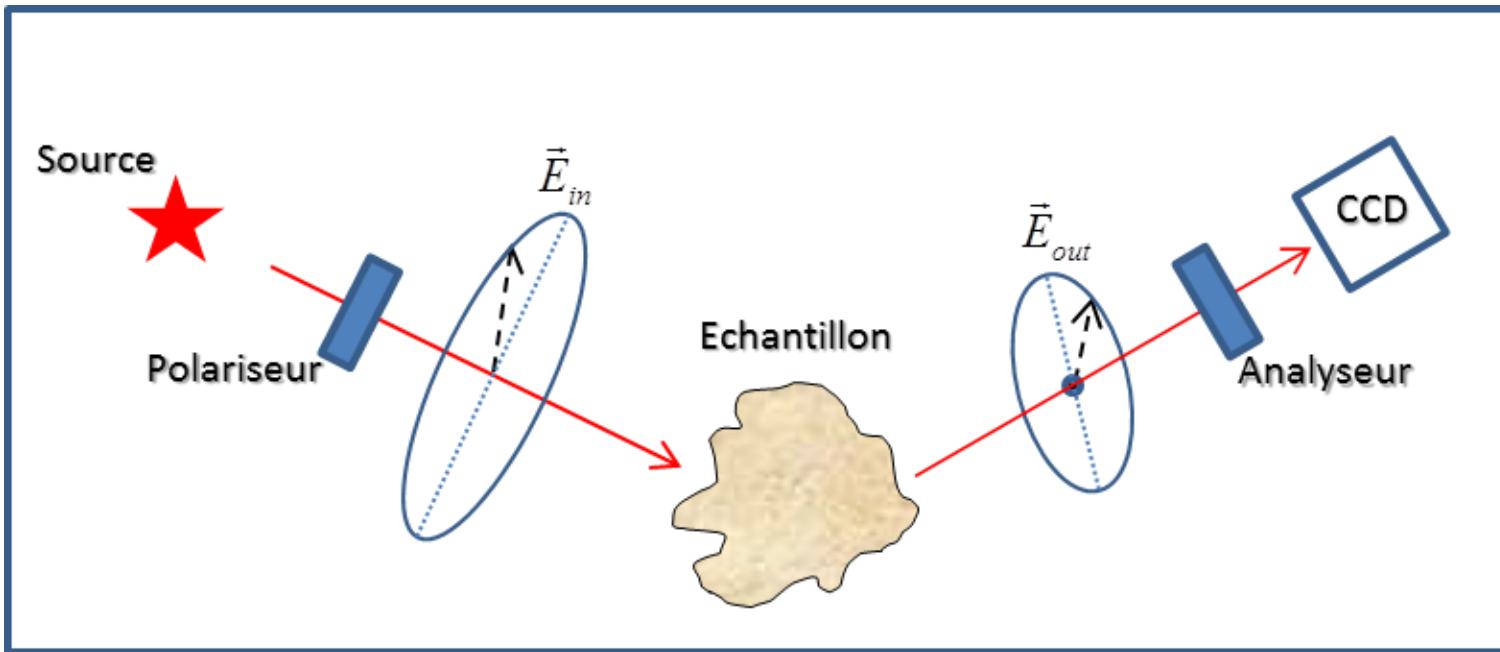
2. PostDoc and current position 2018-now

Team of Jihad Zallat

- Optical biopsy for skin cancer
- Valorisation through the Poladerme start-up



Polarimetry

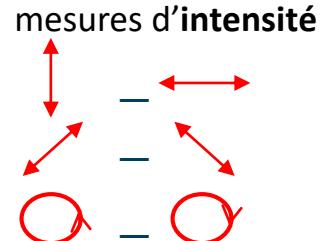


Caractérisation complète de la réponse polarimétrique : la
Matrice de Mueller

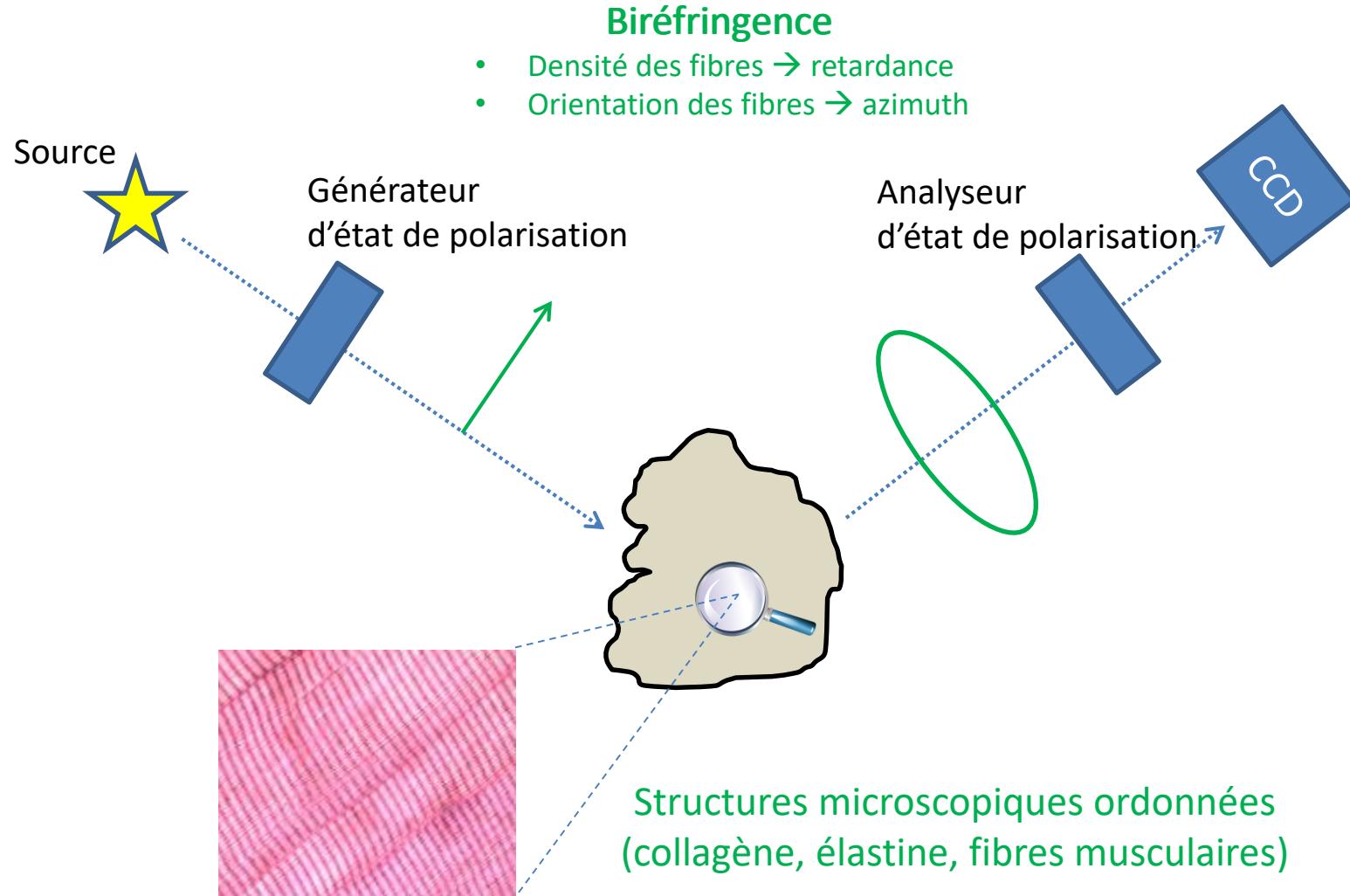
$$\mathbf{S}_{out} = \mathbf{M} \times \mathbf{S}_{in}$$

$\in \mathbb{M}_{4,4}$

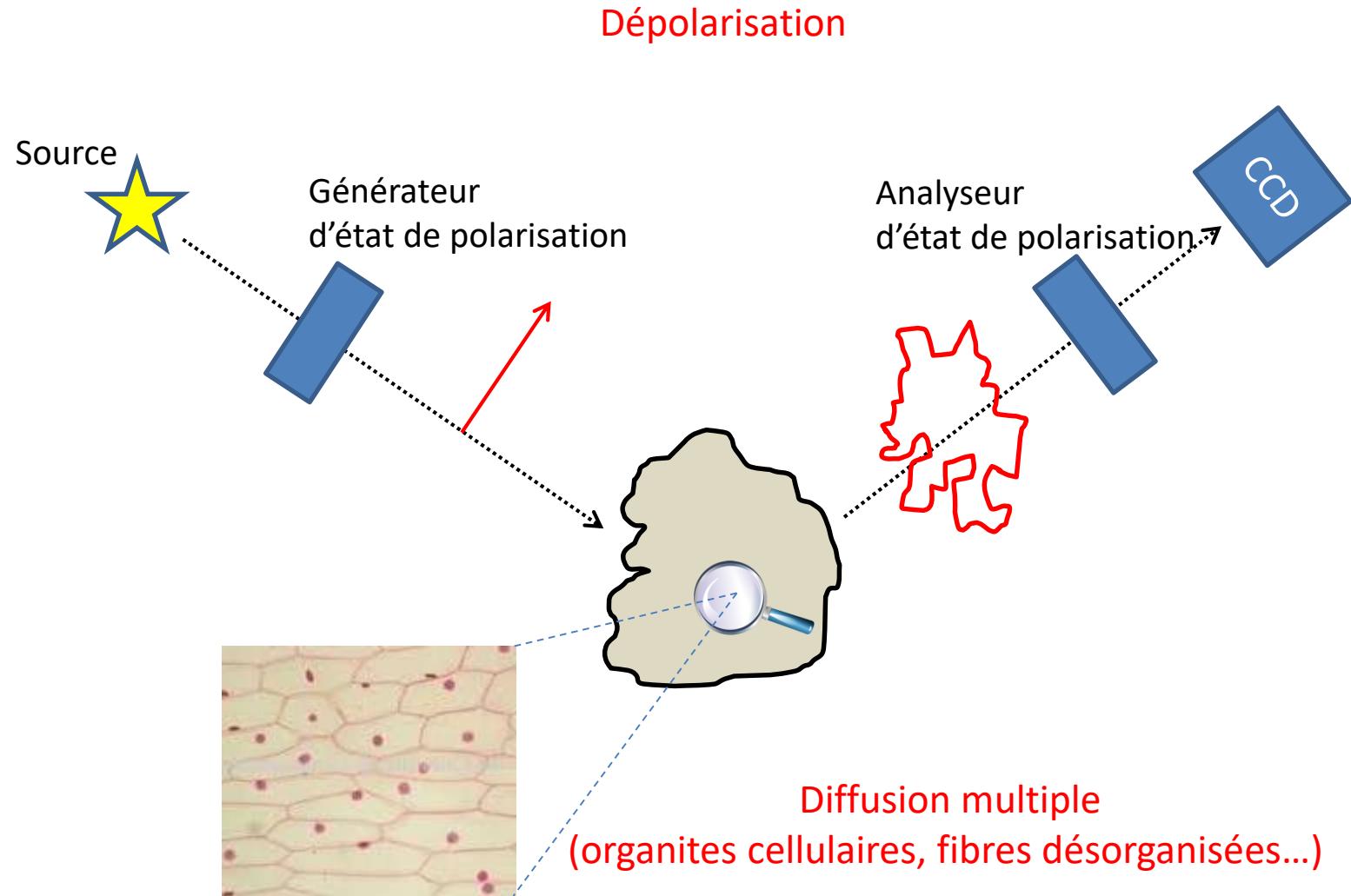
$$\mathbf{S} = \begin{bmatrix} S_0 \\ S_1 \\ S_2 \\ S_3 \end{bmatrix} = \begin{bmatrix} I \\ I_x - I_y \\ I_{+45^\circ} - I_{-45^\circ} \\ I_L - I_R \end{bmatrix}$$



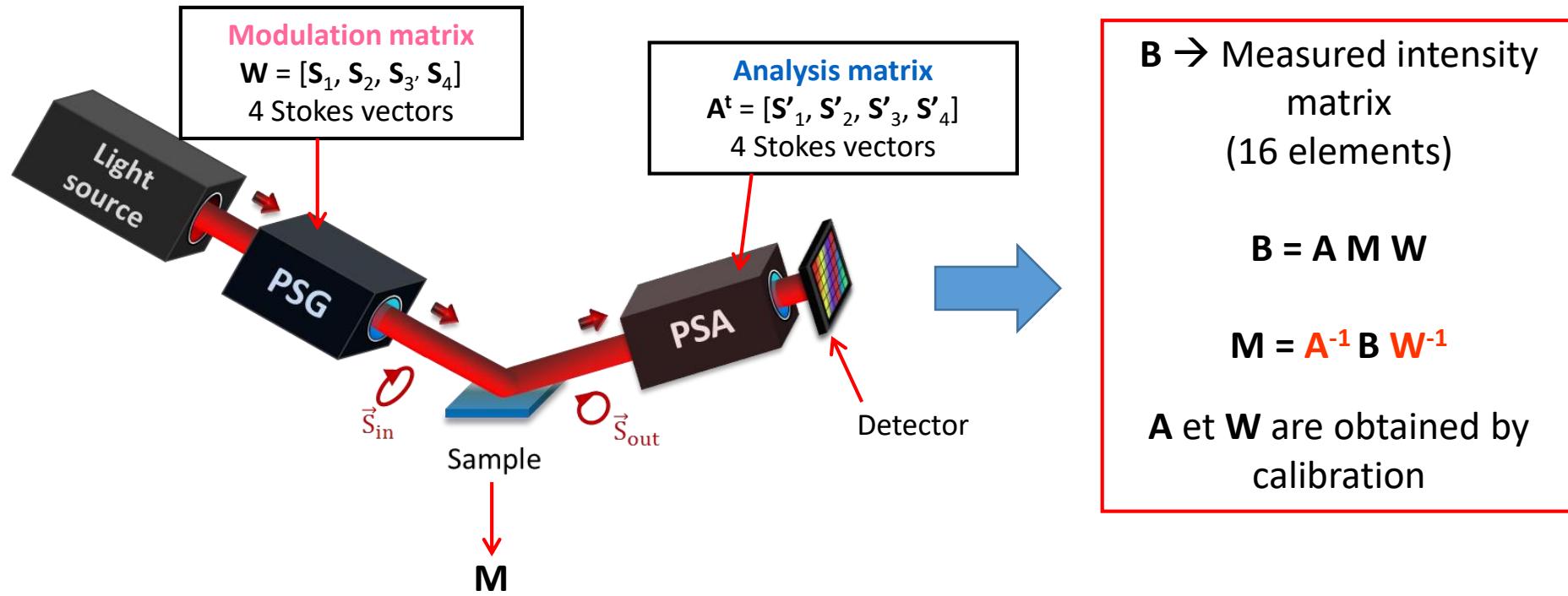
Polarimetric properties of tissues



Polarimetric properties of tissues



Measurement of the Mueller matrix



Eigenvalues Calibration Method (ECM)

- Uses well-known polarization optical elements (polarizers, waveplates, etc.)
- No a priori modelling of the instrument needed

Advantages of Mueller polarimetric imaging

- Wide field ($\sim 5 \times 5 \text{ cm}^2$)
- Fast acquisition speed (0.25~1s)
- It explores both optical anisotropy (retardance) and scattering (depolarization) properties at the same time
- Scattering properties from deep depth ($\sim 1 \text{ cm}$, 650nm)⁷
- Bio-safe (visible light)

Preterm birth: birth before 37 amenorrhea weeks

- Preterm birth was responsible for **~1 million perinatal deaths** in 2015¹
- **Current diagnostics:** measurements of cervical length shortening
 - 1~2 echographies per week²
 - Low diagnostic performance of the current method: ~50% women hospitalized for threatened preterm birth have actual preterm birth³
- **The goal:** development of a new diagnostic tool to improve the diagnosis of preterm birth

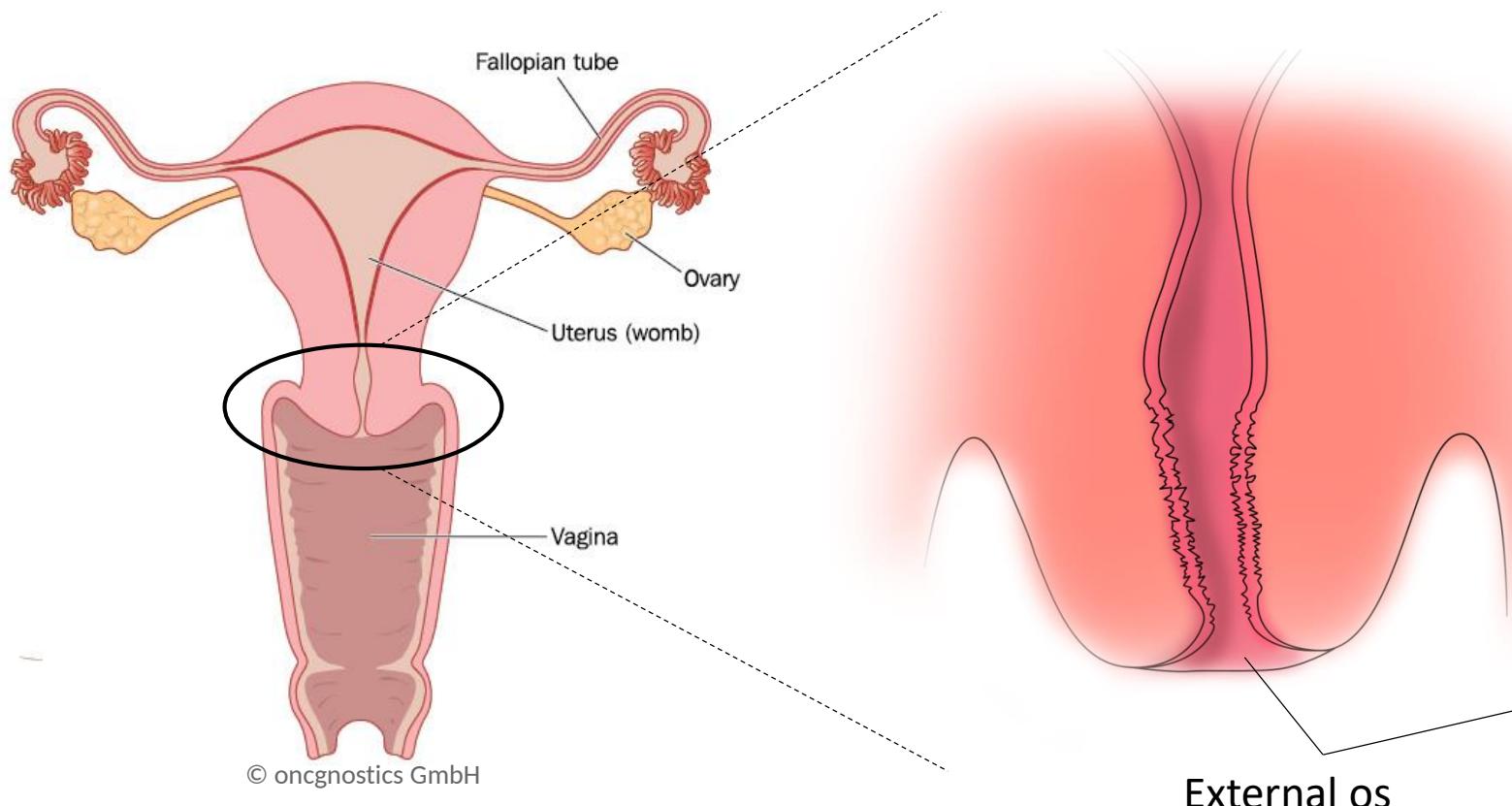
1. Liu, L., et al., Lancet **388**(10063), 3027–3035 (2016).

2. Lim, K., et al., J. Obstet. Gynaecol. Canada **40**(2), e151–e164 (2018).

3. McPheevers, M. L., et al., Am. J. Obstet. Gynecol. **192**(4), 1325–1329, Mosby Inc. (2005).

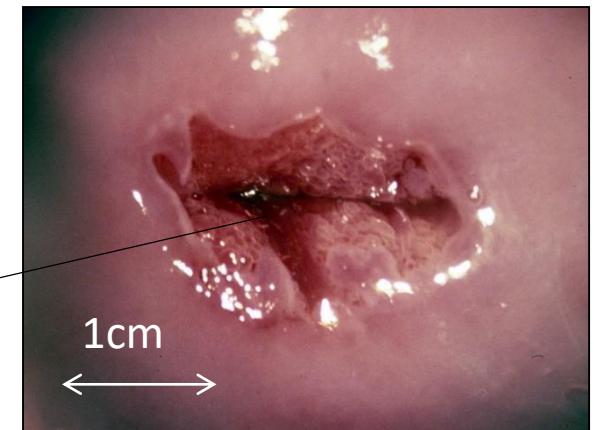
The cervix: the orifice of the uterus

It mechanically keeps the fetus in the uterus



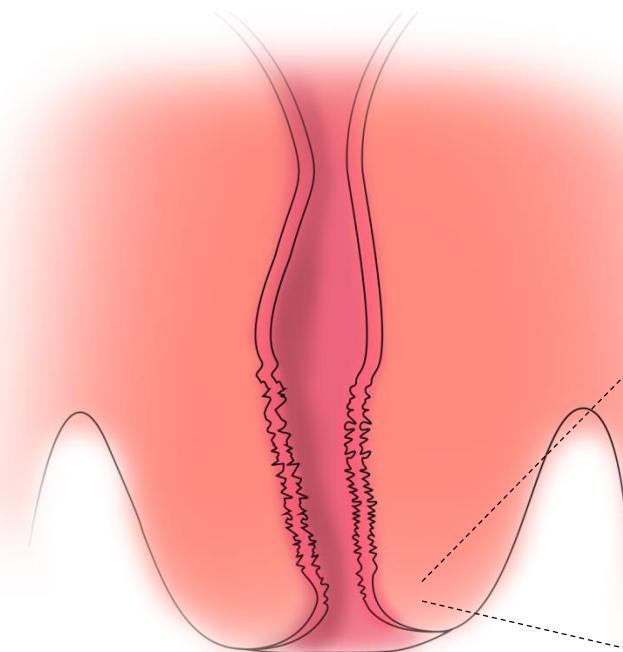
External os

Cervix – frontal view

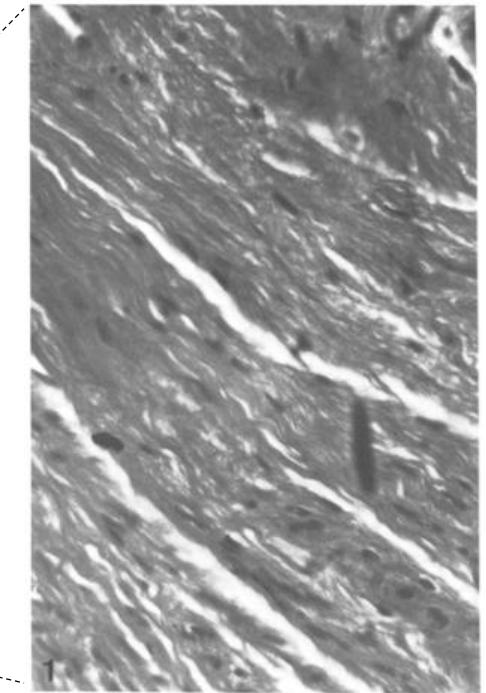


The cervix: the orifice of the uterus

It mechanically keeps the fetus in the uterus



P. W. Theobald (1982)

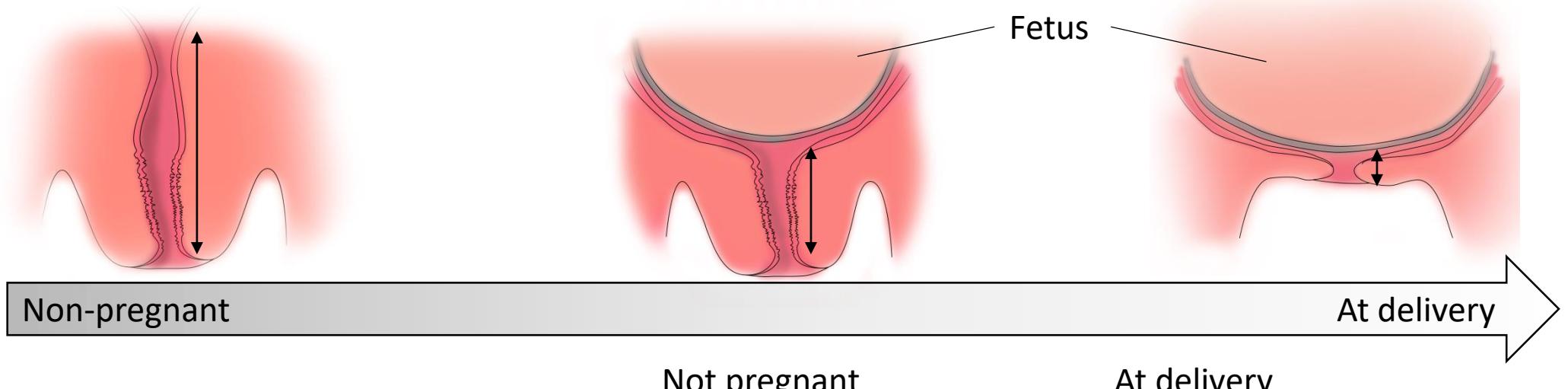


Collagen plays an important role in mechanical properties of tissues

Collagenous connective tissue
80% – Collagen
(70% type I, 30% type II collagen)

Changes of the cervix during pregnancy

Macroscopic changes



Microscopic changes

Hydration ⁴	↑	75%	81%
Collagen density ⁵	↓		
Collagen solubility ⁴	↑	32~40%	80%
Stiffness ⁶	↓	320±120 mbar	53±26 mbar

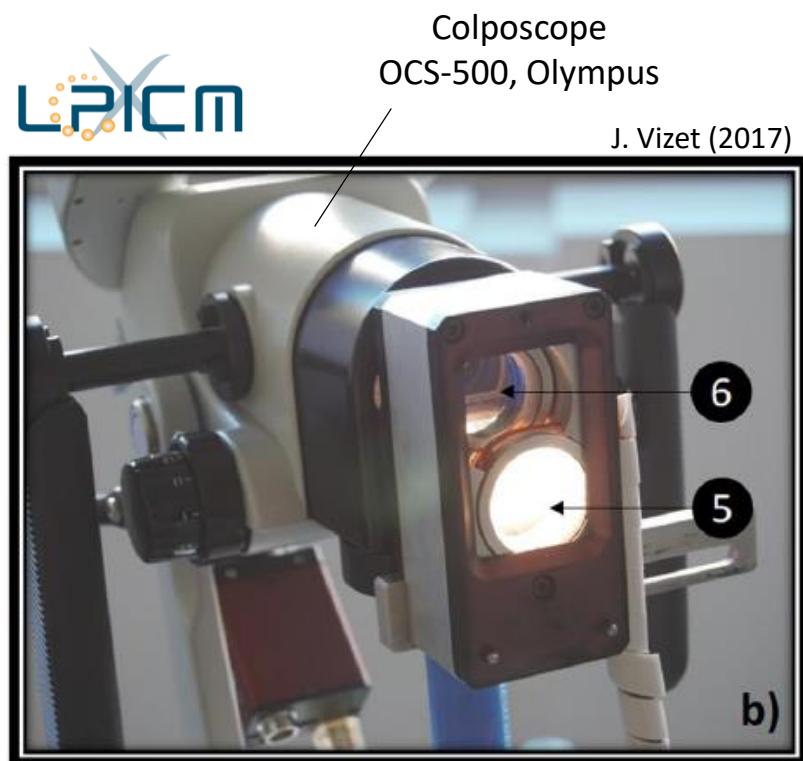
4. Myers, K., et al., Eur. J. Obstet. Gynecol. Reprod. Biol. **144**, S82–S89 (2009).

5. Akins, M., et al., J. Biomed. Opt. **15**(2), 026020 (2010).

6. Badir, S., et al., Prenat. Diagn. **33**(8), 737–741 (2013)

The Mueller polarimetric colposcope (MPC)

The PSG and PSA are grafted on a colposcope



The Mueller polarimetric colposcope
(5-PSG, 6-PSA)

Specifications of imaging system

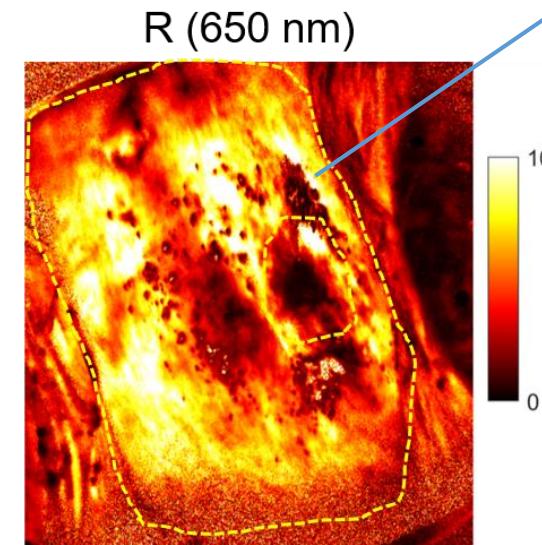
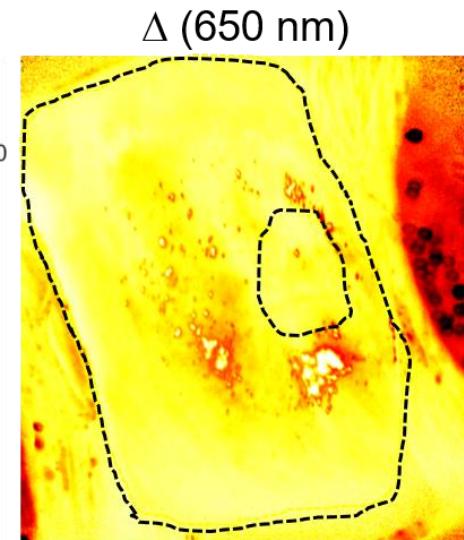
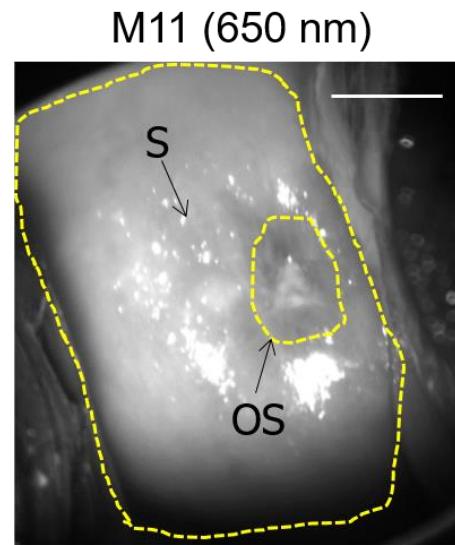
- Resolution: 800 X 600 pixels
- Field of view: 4X3 cm²
- Wavelength: 650nm (FWHM: 40nm)
- FPS: 24 frames/s
- Light source: 300W Xenon

Data collection: 24 individual pregnant women

- A single examination for each patient
- Gestational age: 20-39 weeks
- Age: 16 – 41
- Primigravida: 12
- Multigravida: 12
- All timely delivered
- At the Brugmann university hospital in Brussels

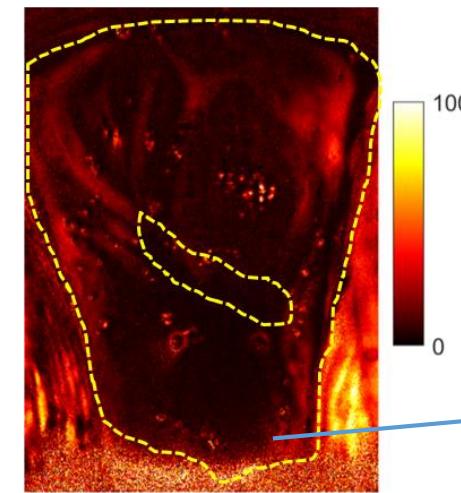
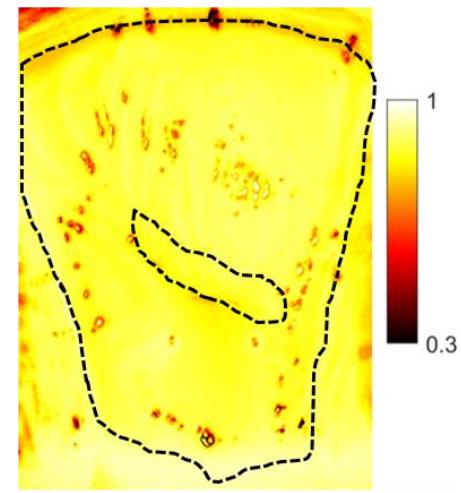
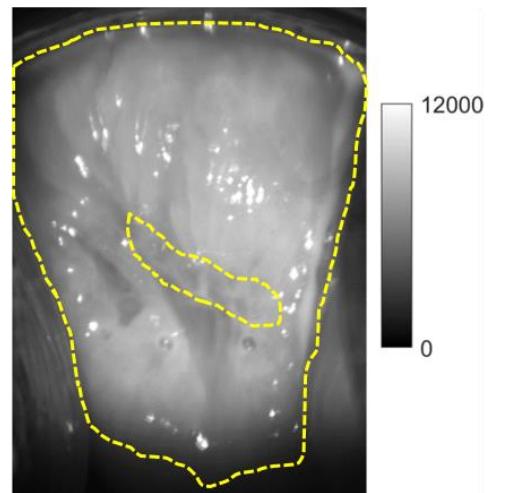


Polarimetric contrasts for 2 patients



Squamous epithelium

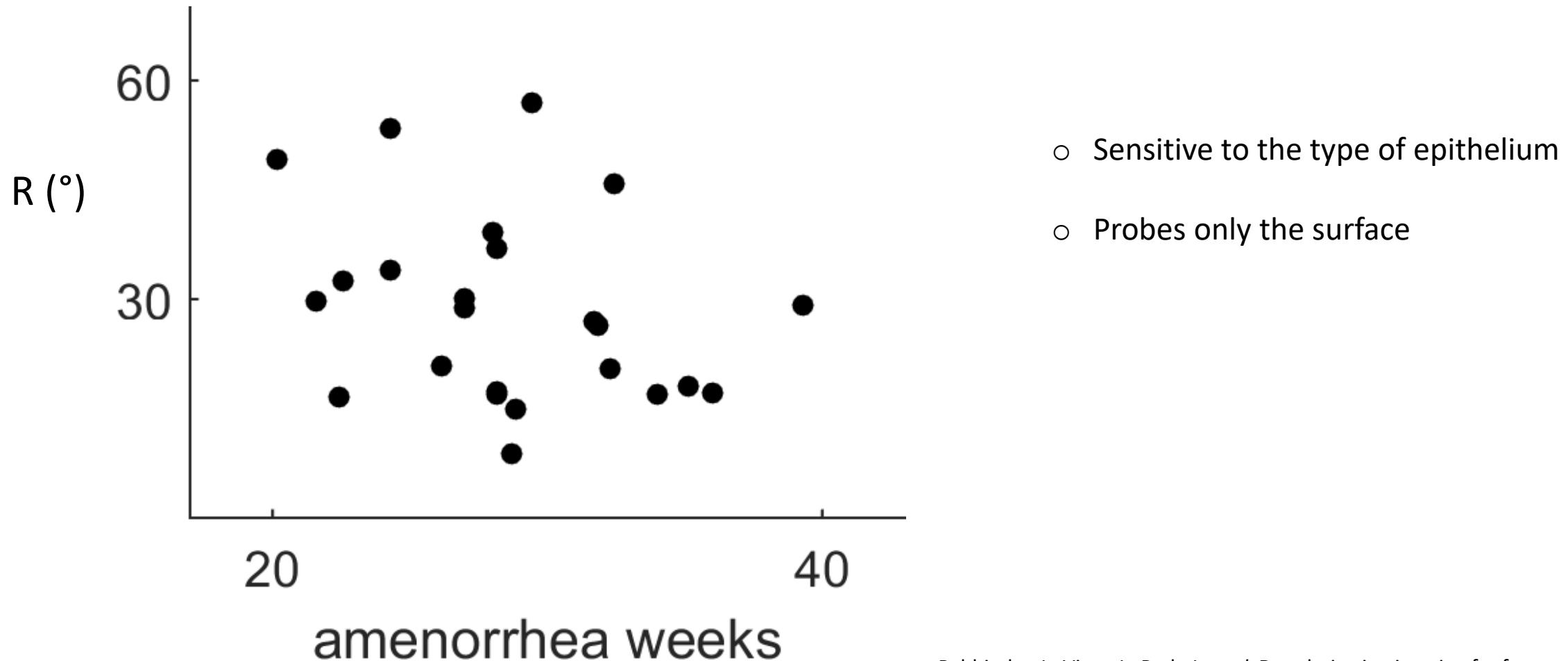
Patient 1
29 weeks of amenorrhea and 3 days



Patient 2
28 weeks of amenorrhea and 5 days

Standardization of the term birth

Retardance does not correlate with gestational age

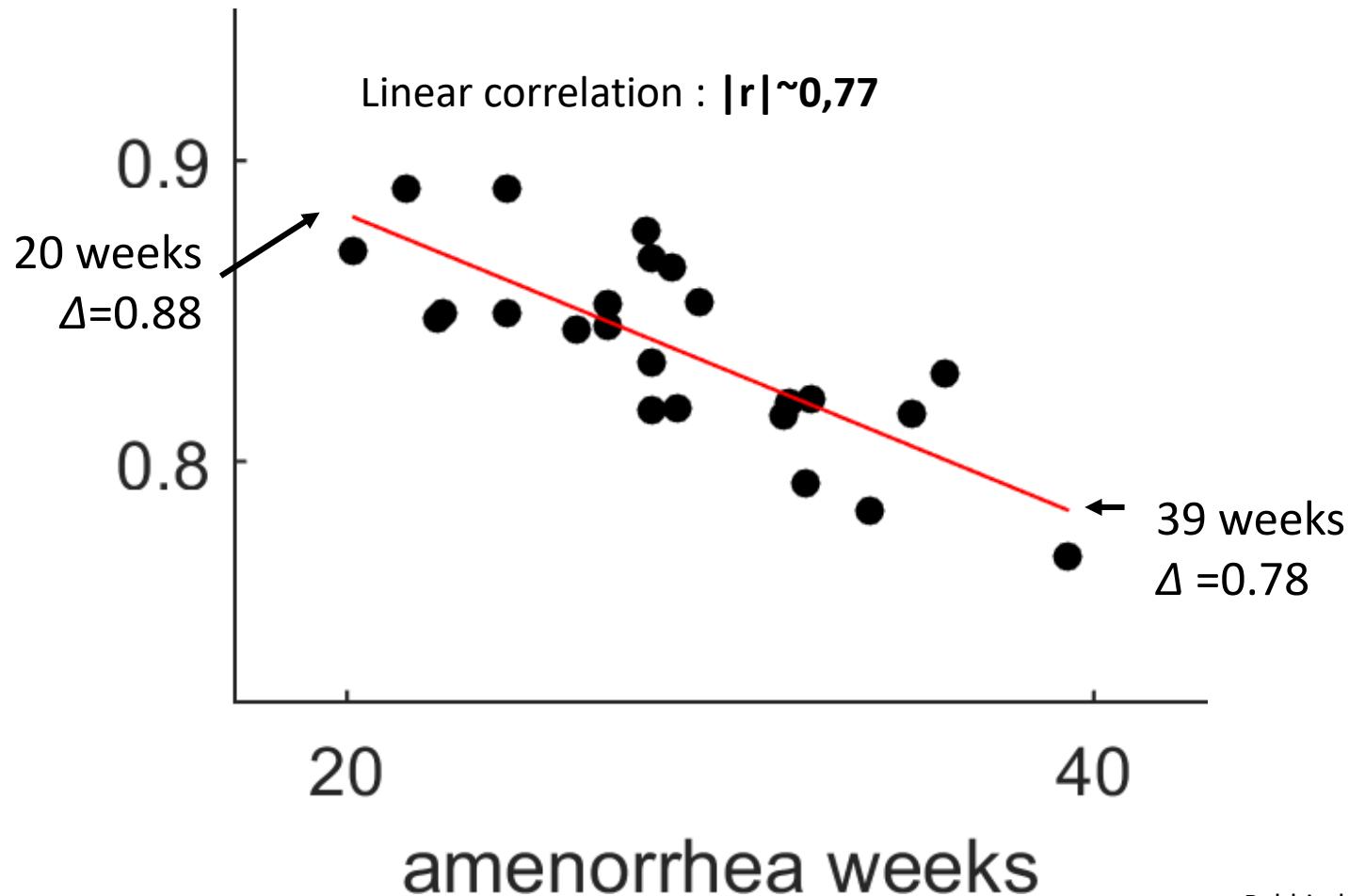


○ Sensitive to the type of epithelium

○ Probes only the surface

Standardization of the term birth

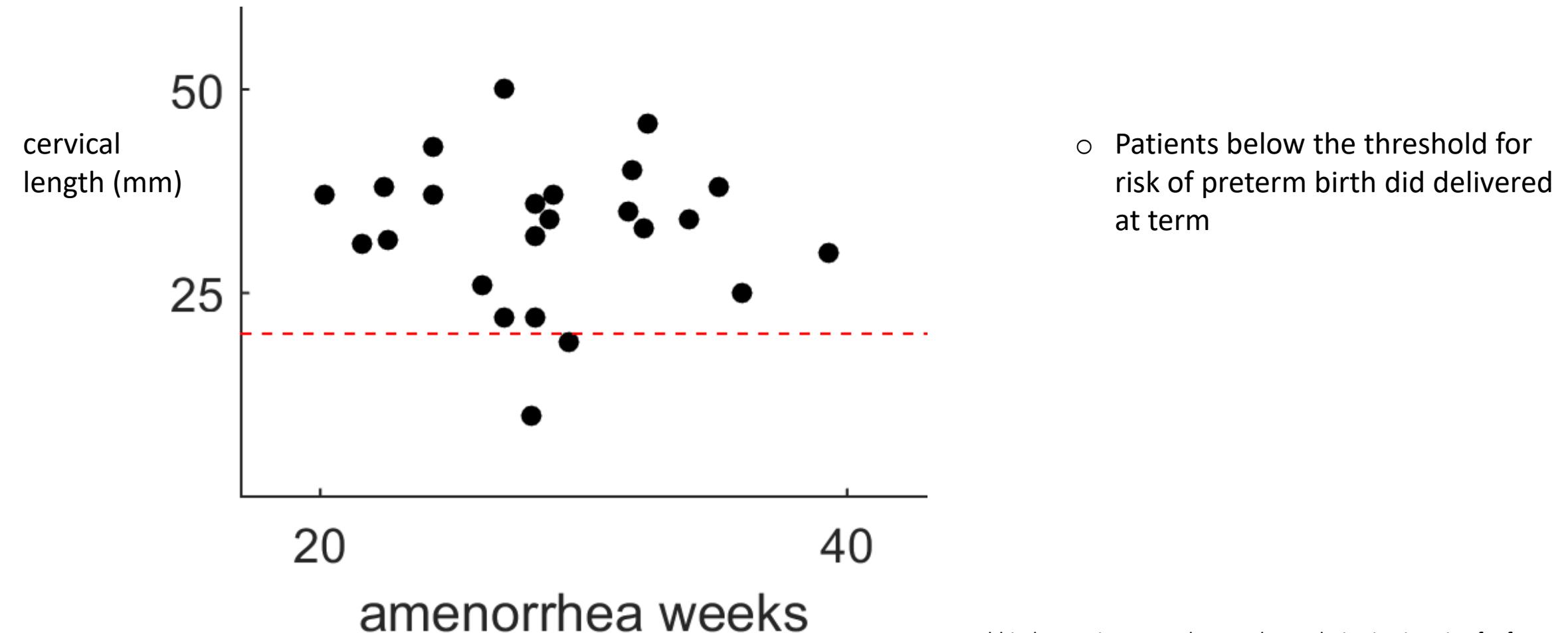
The cervix is losing depolarizing ability over the pregnancy



- Increased hydration¹
(particle density ↓)
- Decreased collagen density²
- Probes the volume scattering properties (less sensitive to the surface structure)

Standardization of the term birth

We have observed no trend in cervical length measurements



Rehbinder, J., Vizet, J., Park, J. et al. Depolarization imaging for fast and non-invasive

monitoring of cervical microstructure remodeling in vivo during pregnancy. *Sci Rep* **12**, 12321 (2022).

Conclusion preterm birth

- The **depolarization** of the cervical tissue is decreasing during pregnancy.
- It reflects the cervical maturation during pregnancy.
- The depolarization parameter at **650 nm** is promising to define a standardization curve on a cohort of patient to follow the steady progression of pregnancy.
- A clinical study of 2 groups (normal vs preterm) is being carried out to figure out the longitudinal changes on 650 patients.



ANR Digit MC-PB

Clinical study *in vivo* on 650 patients
(2000 Colposcopies)
Started december 2020 (Duration 36 mois)



Polarimetry at ICube (Strasbourg)

- 1 • Polarization imaging at LSIIIT in 1997
• Construction of several instruments
• Medical applications: data processing, collaboration with LPICM, ANR
- 2 • Patent for ultra-stable modulators
• POLARIS project (SATT)
• SATT : Transfer (IHU, Aesculap, Sakura, Storz, ...)
- 3 • SATT maturation support (Dermapol project)
• Clinical trial
• ARCHOS and creation of POLADERME in October 2021
• Filing of a new patent for the POLADERME solution
• POLADERM is owned by MDV and listed on the stock exchange on 10/02/2022

Polarimetry at ICube (Strasbourg)



POLARIS

Evolution of the prototypes



Dermapol

Dermatoscope connecté
(startup Poladerme)



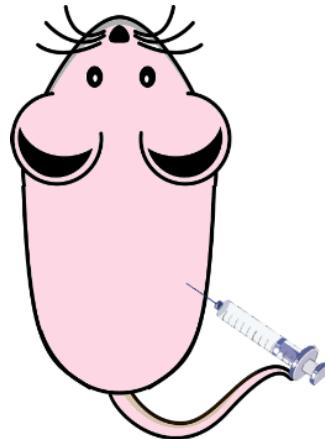
Polarimetry at ICube (Strasbourg)

POLARIS	Dermapol	Dermatoscope connecté
Preuve de concept <ul style="list-style-type: none">• ~1 m x 1 m• ~50-100 k€• Statique <ul style="list-style-type: none">• Image de Mueller complète• Caméra scientifique• Mesures ex-vivo	Etude sur le petit animal et étude clinique <ul style="list-style-type: none">• ~50 cm x 10 cm• ~20-25 k€• Transportable	Industrialisation <ul style="list-style-type: none">• ~10 cm x 5 cm• <100 €• Connecté <ul style="list-style-type: none">• Etats de polarisation discrets + stéréo-photométrie• + stéreo-vision• 5 caméras smartphone• Machine learning, IA

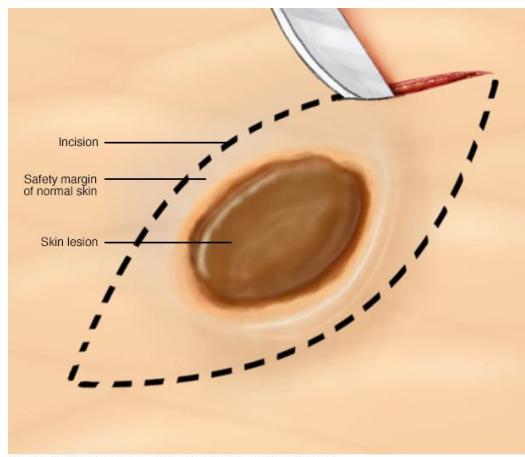
Dermapol



- **Non-invasive**
- **Sensitive to the organisation of the tissue**
- **Label-free**
- **Quick measurement**



evolution of grafted tumors in mice with and without treatment



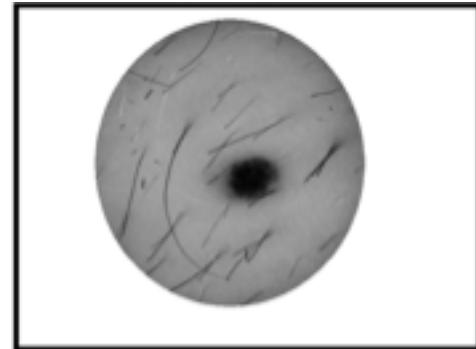
Clinical trial at Hôpital Civil of Strasbourg

Acquisition on all types of skin lesions, before biopsy

Polarimetric signatures for skin lesions

Visuel standard

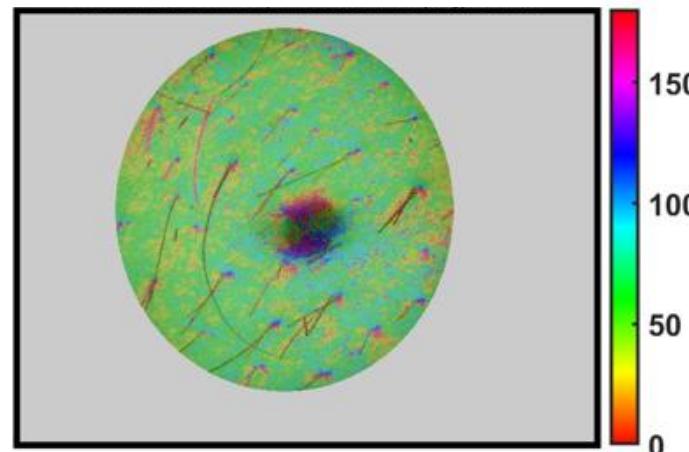
Intensité



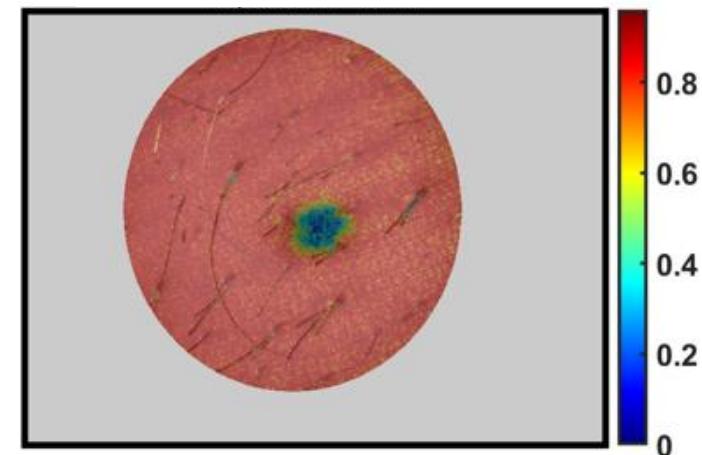
Naevus

POLADERME

Orientation de l'axe rapide du retardeur (deg) – 680 nm



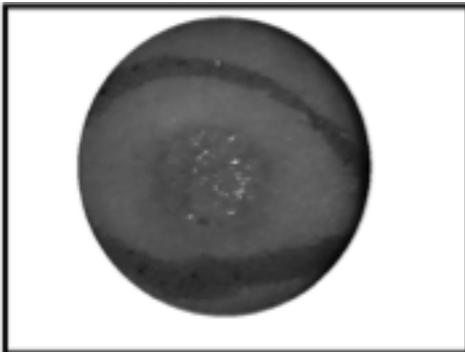
Dépolarisation – 680 nm



Polarimetric signatures for skin lesions

Visuel standard

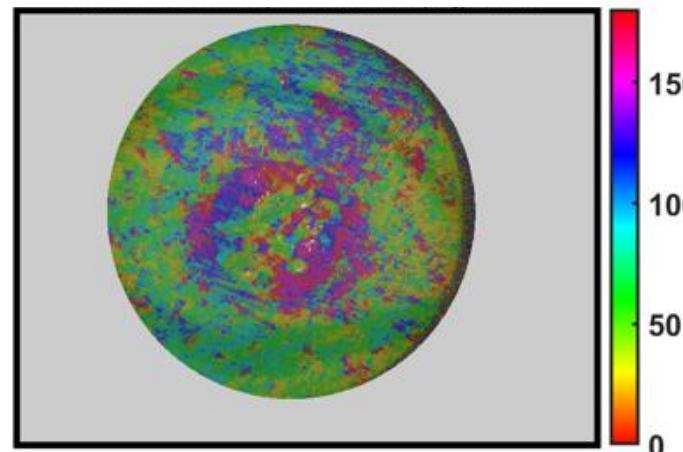
Intensité



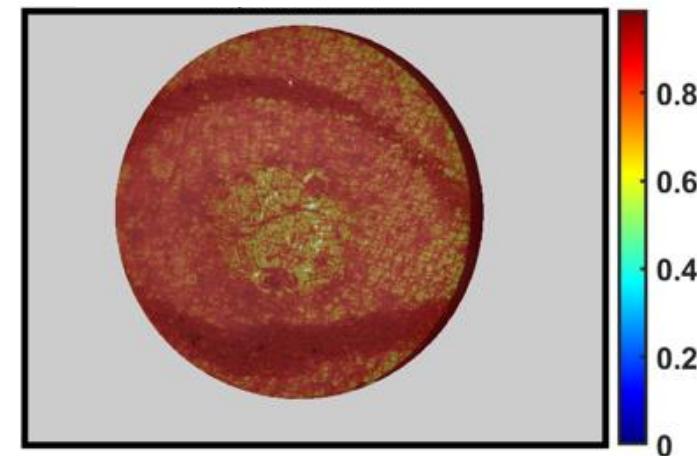
Carcinome
basocellulaire

POLADERME

Orientation de l'axe rapide du
retardeur (deg) – 680 nm



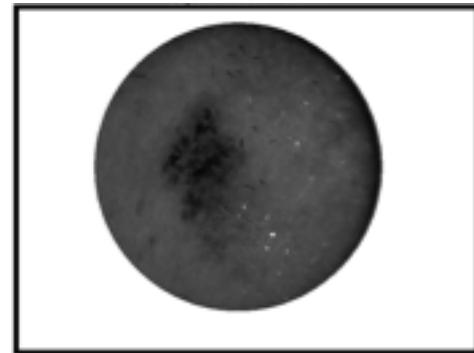
Dépolarisation – 680 nm



Polarimetric signatures for skin lesions

Visuel standard

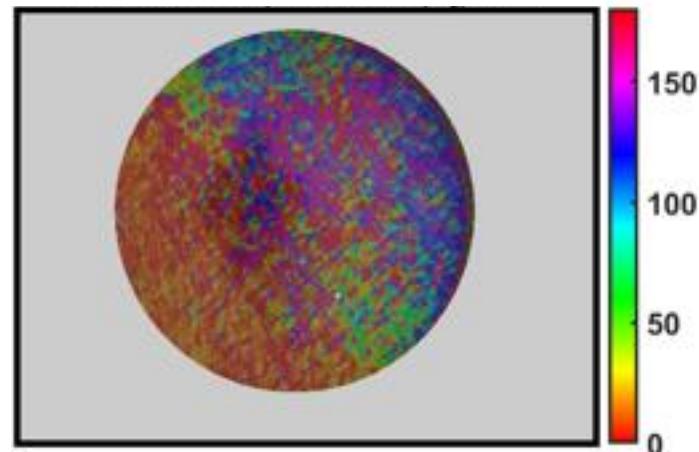
Intensité



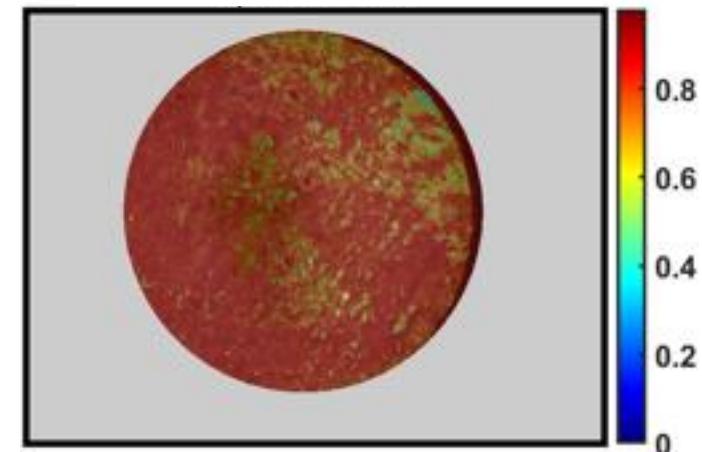
Mélanome

POLADERME

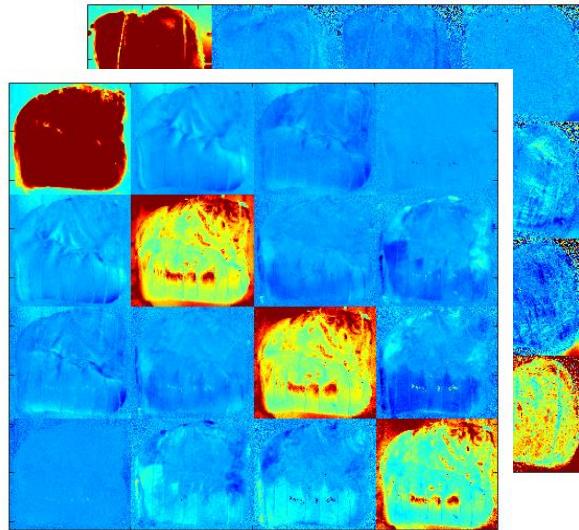
Orientation de l'axe rapide du retardeur (deg) – 680 nm



Dépolarisation – 680 nm

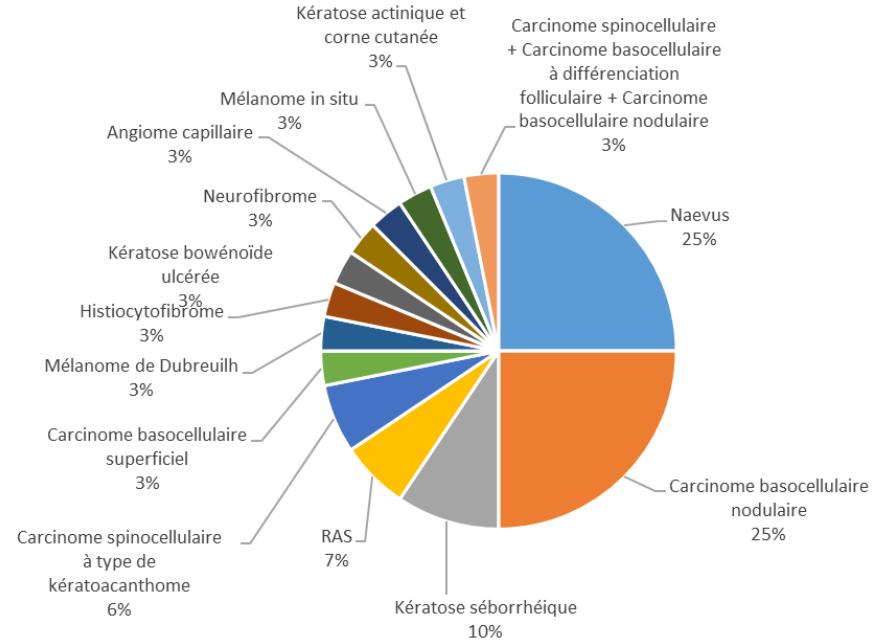


Polarimetry and machine-learning



Database of polarimetric images

...



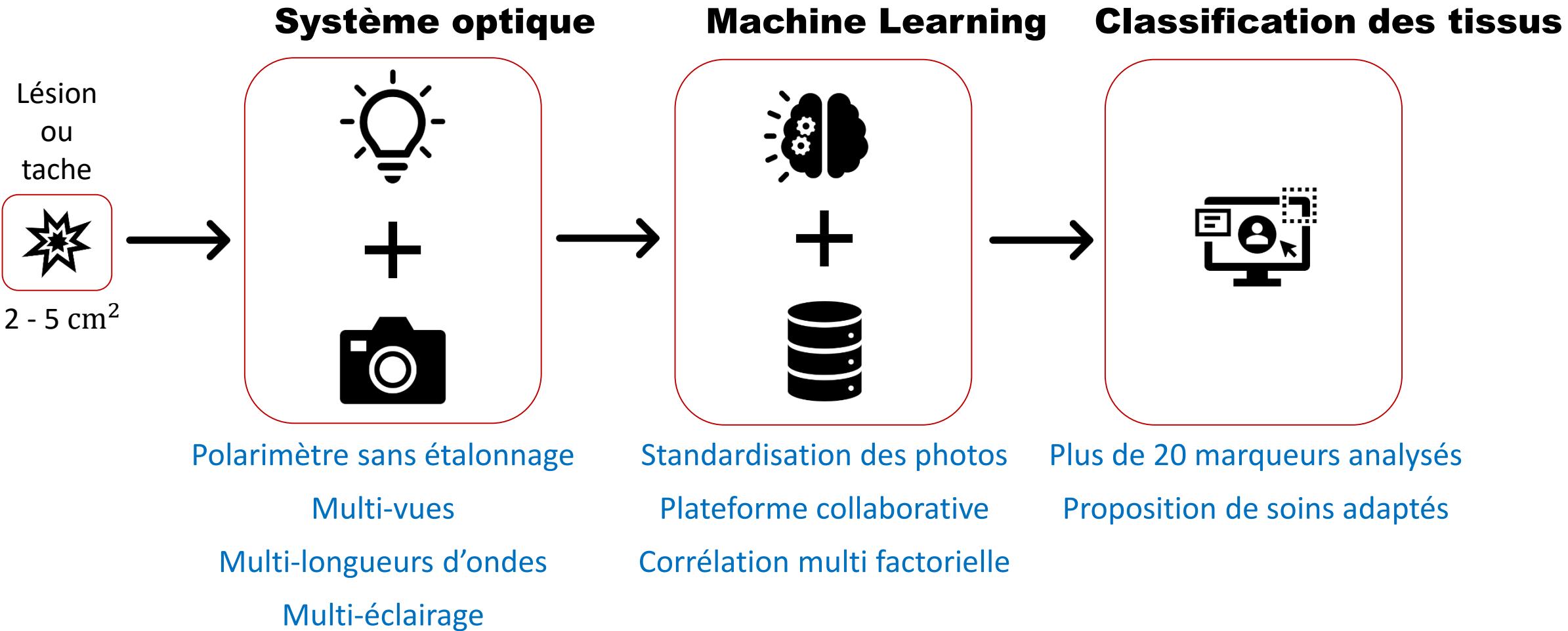
Ground truth labelling

Problem : Scarcity of (clinical) data

- Complexity of the prototype
- Manpower for data collection
- Ground truth expensive (histology)



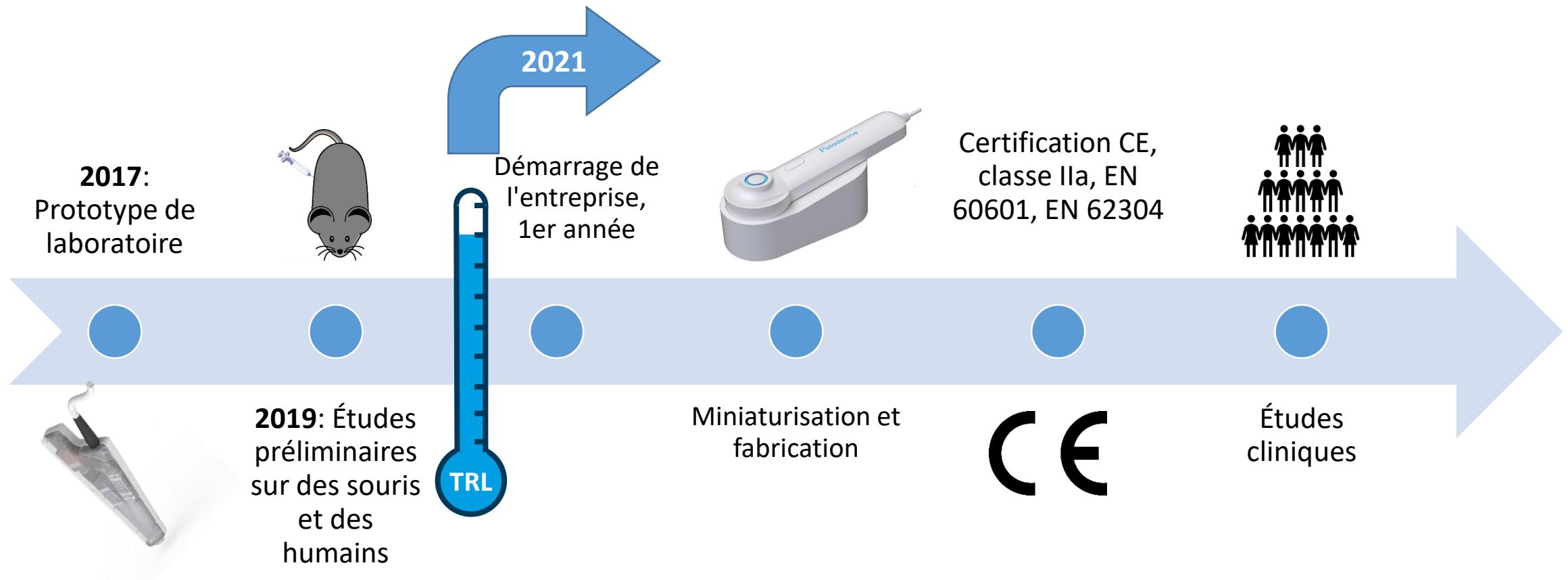
La solution Poladerme



Conclusion Poladerme

	Dermatoscope	POLADERME
Grossissement	✓	✓
Éclairage	✓	✓
Analyse de la qualité du collagène	✗	✓
Vascularisation	✗	✓
État de surface de la peau	✗	✓
Orientation des fibres	✗	✓
Information biomécanique	✗	✓

Outlook Poladerme



« Take-home » messages

Optical Imaging can provide:

- Label-free contrasts, sensitive to the micro-organization and chemical composition of tissues !
- Histological insights *in-vivo* !
- Video-rate imaging !
- A broad range of complementary techniques (not all described in this talk)

Limitations and challenges:

- “Medical is hard” – technical hurdles + tricky to find the right business model + slow adoption of new techniques
- What can be published ≠ what can be marketed

A bright future for optical medical imaging

Optical Biopsy:

- Optical imaging for prevention/screening, conventional medical imaging for treatment
- “Virtual staining” for histopathology
- Low-resource settings

ML&AI:

- Increased information content through optical techniques → diagnostic aid extracted using machine-learning algorithms

Point-of-Care testing:

- Shortage of doctors, medical deserts
- Availability of smartphones (light source + camera + computing power)

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